# Enzymatic synthesis and characterization of grafted polyesters and their use as steric stabilizers for cubosomes

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## **TABLE OF CONTENTS**

1	IN	TRODUCT	ION	1
	1.1	ENZYMA	TIC POLYESTER SYNTHESIS AND GRAFTING	1
	1	1.1 Lip	ases	1
	1.3	1.2 Enz	zymatic synthesis of functional polyesters	4
	1.2	1.3 Gr	nfting of functional polyesters	6
	1.2		IENTALS OF LIPID SELF-ASSEMBLY	
	1.2	2.1 Lip	id polymorphism	10
		1.2.1.1	The lamellar phase	
		1.2.1.2	The hexagonal phase	
		1.2.1.3		
		1.2.1.4	Bicontinuous phases	13
		1.1.1.1	.1 The sponge phase	13
		1.1.1.1		
	1.2	2.2 Bin	ary phase diagram of GMO-water system	16
	1.2	2.3 The	e effect of additives on the mesophase behavior of the GMO-water system	18
	1.3	STERIC ST	TABILIZERS FOR CUBOSMES	20
	1.4	AIMS AN	D OBJECTIVES	22
2	FA	TTY ACID	MODIFIED SUGAR BASED POLYESTERS	24
	2.1	INTRODU	JCTION	24
	2.2	Experime	NTAL PART	26
	2.2		iterials	
	2.2		itheses	
		2.2.2.1	Synthesis of poly(xylitol adipate)	
		2.2.2.2	Synthesis of poly(D-sorbitol adipate)	
		2.2.2.3	Synthesis of stearoyl grafted poly(xylitol adipate) and poly(D-sorbitol adipate)	
	2.2	2.3 Pre	paration of nanoparticles	27
	2.2	2.4 Ins	trumentation	28
		2.2.4.1	NMR spectroscopy	28
		2.2.4.2	Size exclusion chromatography (SEC)	28
		2.2.4.3	Differential scanning calorimetry (DSC)	28
		2.2.4.4	Dynamic light scattering (DLS)	28
		2.2.4.5	Negative-staining TEM	29
		2.2.4.6	X-ray diffraction (XRD)	29
	2.3	RESULTS A	ND DISCUSSION	29
	2.3	3.1 Poi	ymerization and grafting	29
	2.3	3.2 Na	noparticles	35
		2.3.2.1	Dynamic light scattering	35
		2.3.2.2	Negative-staining transmission electron microscopy	36
	2.4	Conclusion	DNS	37
3	PC	DLY(GLYCI	EROL ADIPATE)-G-OLEATE AND THE GMO/WATER SYSTEM	38
	3.1	INTRODU	JCTION	38
	3.2	Experime	NTAL SECTION	41
	3.2	2.1 Ma	iterials	41
	3.2		ntheses	

3.2.2			
	3.2.2.	-, , -, -, -	
	3.2.2.	.,	
	3.2.3	Polymer characterization	
	3.2.4	Sample preparation for X-ray diffraction	43
	3.2.5	Preparation of nanoparticles	
	3.2.6	Dynamic light scattering	44
	3.2.7	Negative stain transmission electron microscopy	44
	3.2.8	Cryogenic transmission electron microscopy	45
	3.2.9	X-ray diffraction	45
	3.3 RESUI	TS AND DISCUSSION	46
	3.3.1	Syntheses and grafting of poly(glycerol adipate) and glycerol monooleate	46
	3.3.2	Characterization of PGA-g-Ox with nanodomains formed by oleate side chains	51
	3.3.3	The ternary system GMO/PGA-g-O22/water	53
	3.3.4	PGA-g-O22 as a potential stabilizer for GMO based nanoparticles in aqueous dispersions	61
	3.4 CON	CLUSION	63
	NALU TIC	DAFT DOLVESTEDS AS STABILIZEDS FOR SUROSOMES	c.
4	MULTIG	RAFT POLYESTERS AS STABILIZERS FOR CUBOSOMES	65
	4.1 INTR	ODUCTION	65
	4.2 EXPE	RIMENTAL PART	67
	4.2.1	Materials	67
	4.2.2	Syntheses	68
	4.2.2.	1 Carboxylation of mPEG750 and mPEG1K	68
	4.2.2.	0 - p - 7,0 / p	
	4.2.2.		
	4.2.2.	,	
	4.2.2.		
	4.2.2.		_
	4.2.2.	,	
	4.2.3	Preparation of cubosome dispersions	
		LTS AND DISCUSSION	
		Polymer synthesis and grafting	
	4.3.2	Graft copolymers as steric stabilizers of cubosomes	
	4.4 CONC	LUSION	82
5	SUMMA	\RY	83
6	REFERE	NCES	86
7	APPEND	XIX	100
8	ACKNO	<i>N</i> LEDGMENT	105
9		ULUM VITAE	
10		PUBLICATIONS	
11		TÄNDIGKEITSERKLÄRUNG	

#### ABBREVIATIONS AND SYMBOLS

#### **ABBREVIATIONS**

Asp Aspartic acid

ATRP Atom transfer radical polymerization

CAC Critical aggregation concentration

CAL-B Candida antarctica Lipase B

CMC Critical micelle concentration

CMT Critical micelle temperature

CPP Critical packing parameter

DCM Dichloromethane

DDS Drug delivery system

DMAP 4-Dimethylaminopyridine

DMPE 1,2-Dimyristoyl-*sn*-glycerol-3-phosphoethanolamine

DMSO Dimethyl sulfoxide

DOPE 1,2-Dioleoyl-*sn*-glycerol-3-phosphoethanolamine

DSC Differential scanning calorimetry

DSPE 1,2-Distearoyl-*sn*-glycerol-3-phosphoethanolamine

EDC 1-Ethyl-3-(3-dimethylaminopropyl)carbodiimide

eROP Enzymatic ring opening polymerization

FA Fatty acid

FI Fluid isotropic

G1MO Glycerol-1-monooleate

G2MO Glycerol-2-monooleate

Gln Glutamine

Glu Glutamic acid

GMO Glycerol monooleate, monoolein

His Histidine

LLC

HLB Hydrophilic to lipophilic balance

IPMS Infinite periodic minimal surface

Lyotropic liquid crystal

MAG Monoacyl glycerol

MO Monoolein

NP Nanoparticle

PBS Poly(butylene succinate)

P(ODA-b- Poly(octadecyl acrylate)-block-poly(ethylene glycol monomethyl ether

P(PEGA- acrylate)

OME))

PC Diacyl phosphatidyl choline

PCL Poly( $\varepsilon$ -caprolactone)
PDI Polydispersity index

PDSA Poly(D-sorbitol adipate)

PDSA-*g*-Sx Poly(D-sorbitol adipate)-*graft*-stearate, x stands for mol% grafting of

OH groups of polymer backbone with stearate side chain

PEG Poly(ethylene glycol)

PGMA Poly(glycerol methacrylate)

PEI Poly(ethylene imine)
PEO Poly(ethylene oxide)
PGA Poly(glycerol adipate)

PGA-*g*-Ox Oleate grafted poly(glycerol adipate) where x is the mol% grafting of

PGA with oleate side chians

 $PGA_xO_yPEG_z$  Oleate and PEG grafted poly(glycerol adipate), where x is the degree of

polymerization of PGA, y and z stand for the number of oleate and PEG

side chains, respectively.

PGS Poly(glycerol sebacate)

PLA Poly(lactic acid)

PPO Poly(propylene oxide)

PXA Poly(xylitol adipate)

PXA-g-Sx Poly(xylitol adipate)-graft-stearate, x stands for mol% grafting of OH

groups of polymer backbone with stearate side chain

RAFT Reversible addition-fragmentation chain transfer polymerization

RI Refractive index

ROP Ring opening polymerization
SAXS Small angle X-ray scattering

SEC Size exclusion chromatography

Ser Serine

TEM Transmission electron microscopy

Thr Threonine

WAXS Wide angle X-ray scattering

XRD X-ray diffraction

<sup>1</sup>H NMR Proton nuclear magnetic resonance

13C NMR Carbon-13 nuclear magnetic resonance

#### **SYMBOLS**

 $M_n$  Number average molar mass

 $M_w$  Weight average molar mass

*r*<sub>h</sub> Hydrodynamic radius

 $\Delta G_{agg}$  Gibbs free energy of aggregation

 $\Delta H_{agg}$  Enthalpy of aggregation

 $\Delta S_{agg}$  Entroy of aggregation

*Vi* Volume of amphiphilic molecule

 $l_c$  Length of hydrophobic chain of an amphiphile

*ao* Effective area of head group of an amphiphile

χ Euler-Poincare characteristics

γ Critical packing parameter

*L*<sub>2</sub> Isotropic phase

*H*<sub>2</sub> Reverse hexagonal phase

*Lc* Lamellar crystal phase

 $L_{\alpha}$  Liquid crystalline lamellar phase

 $L_{\beta}$  Lamellar tilted gel phase

 $L_{\beta}$  Lamellar gel phase

 $L_{\beta I}$  Lamellar interdigitated gel phase

 $P_{\beta}$  Lamellar rippled gel phase

Slam Reciprocal spacing for lamellar phase

 $\phi_w$  Volume fraction of water  $H_1$  Normal hexagonal phase

 $L_3$  Sponge phase

 $\phi_{\it lipid}$  Volume fraction of lipid

 $\sigma$  Surface area of the minimal surface per unit volume

 $r_w$  Radius of water channel

N<sub>A</sub> Avogadro's number

 $A_{cs}(l)$  Cross-sectional area per lipid molecule

*Vlipid* Volume of lipid molecule

 $\tilde{v}_{lipid}$  Lipid specific volume

 $\delta$  Chemical shift

#### **CHAPTER 1**

#### 1 INTRODUCTION

#### 1.1 ENZYMATIC POLYESTER SYNTHESIS AND GRAFTING

Aliphatic polyesters are macromolecules in which the respective monomers are connected by ester bonds. Aliphatic polyesters are biodegradable and biocompatible and thus they are considered as ideal materials for biomedical applications, including surgery and medicine.<sup>1,2</sup> Poly(lactic acid) (PLA), and poly(butylene succinate) (PBS) are examples of synthetic polyesters which are already in the market for commercial applications.<sup>3</sup>

There are two methods of polyester synthesis: (a) step-growth polycondensation between diols and diacids / diesters or hydroxyacids / hydroxyesters, and (b) ringopening polymerization (ROP) of cyclic monomers. 4 Both methods have advantages as well as disadvantages. For polycondensation, monomers can be derived from renewable resources and are available at low costs, but this method requires conditions of high temperature and vacuum to remove byproducts in order to shift the condensation equilibrium to the forward direction. These high temperatures and vacuum conditions lead to undesired side reaction such as dehydration of diols and βscission of polyesters to form acid and alkene end groups.<sup>5</sup> On the contrary, there is no byproduct in ring opening polymerization, and it is carried out at relatively mild reaction conditions. However, this process requires a catalyst which is usually a salt of heavy metals such as tin<sup>6</sup> and rare earth metals.<sup>7-9</sup> The complete removal of these catalysts from the finished product is difficult which makes these products less suitable for pharmaceutical applications. However the enzymatic synthesis of polyesters is an environmentally benign process which helps to produce linear polyesters of monomers with multiple functionalities at ambient reaction conditions without danger of metal contamination of the product. 10,11

#### 1.1.1 Lipases

In nature, living organisms such as bacteria e.g. *Pseudomonas cepcia* and *Pseudomonas fluorescens*, and fungi e.g. *Candida cylindracea*, *Aspergillus niger*, *Candida* 

rugosa, Penicillium roqueforti, Rhizopus japonicas, Rhizomucor meihei, Mucor meihei, Candida antarctica and Yarrowia lipolytica etc., produce polyesters for their metabolic need. Their synthesis generally involves *in vivo* lipase-catalyzed chain growth polymerization reaction of activated monomers. Lipases are harvested from these living organisms which could be used further for *in vitro* synthesis of polyesters. Lipases could be derived from animals, (where they hydrolyze ester bond, thus converting triglycerides into glycerol and fatty acids) and could be used for *in vitro* polyester synthesis too. The choice of reaction solvent depends on the lipase origin and the monomer structure. Different types of lipases used for *in vitro* polyester synthesis are comprehensively reviewed by Shoda *et al.* Among all studied lipases for polyester synthesis; Candida antarctica lipase B is found to be the best in terms of reactivity, selectivity, and thermal stability, especially when it is immobilized on a support. 17,18

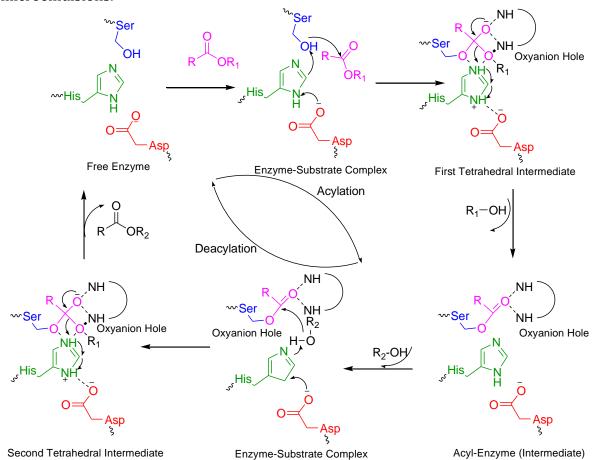
#### Candida antarctica lipase B

Candida antarctica lipase B (CAL-B) is a globular protein that consists of 317 amino acids having a molar mass of 33 kDa. It possesses an  $\alpha/\beta$  hydrolase fold that consists of a  $\beta$ -sheet core of parallel strands connected on both sides by  $\alpha$ -helices, forming an  $\alpha$ - $\beta$ - $\alpha$  sandwich-like shape. Similar to other lipases, CAL-B possesses an active site that is comprised of three amino acids called catalytic triad: a nucleophilic residue (serine), a histidine base and a catalytic acidic residue aspartic acid (Ser105, His224, and Asp187) and it contains two oxyanion holes (Thr40 and Gln106). The active sites of lipases have different shapes, sizes, depth of the pockets, and physiochemical characteristics of their amino acids. The specificity, selectivity and catalytic reactivity of an enzyme depends on its active sites.<sup>19</sup>

A general acylation-deacylation mechanism of lipases is shown in Scheme 1.1. In the acylation step, a proton transfer occurs among the Asp105, His224, and Ser187 residue of the catalytic triad. As a consequence, nucleophilicity of Ser187 increases and it nucleophilically attacks the carbonyl group of the substrate, forming the first tetrahedral intermediate with a negative charge on the oxygen of the carbonyl group. The oxyanion hole is formed by at least one hydrogen bond and is responsible for stabilization of charge distribution as well as the status of the tetrahedral intermediate. In the deacylation step, the enzyme is attacked by a nucleophile (R<sub>2</sub>-OH) resulting in a

new carboxylic acid or carboxylic acid ester with regeneration of enzyme. Hydrolysis occurs when R<sub>2</sub>-OH is water, while alcoholysis occurs when R<sub>2</sub>-OH is an alcohol.<sup>19</sup>

To increase the activity, selectivity, thermal stability, and tolerance for polar organic solvents and facilitate the recycling and reusing, lipases are normally used in their immobilized form.<sup>17,18</sup> Support morphology, surface chemistry, and enzyme packing density largely influence the enzyme activity.<sup>20,21</sup> Lipases can be generally immobilized *via* three different strategies: (1) binding to a solid support (a) by adsorption (by hydrogen bonds or hydrophobic interactions) (b) by ionic binding (e.g. to ion exchange resins), and (c) by covalent binding (e.g. to epoxy groups), (2) crosslinking (e.g. *via* glutaraldehyde), and (3) entrapment (a) in gels (e.g. calcium alginate) (b) in membrane reactors (e.g. hollow fibre reactors), and (c) in reversed micelles of microemulsions.<sup>20,22</sup>



**Scheme 1.1.** Acylation-deacylation mechanism of a lipase.<sup>19</sup>

The most widely used immobilized enzyme is Novozym 435. In the manufacturing of Novozym 435, gene coded lipase is transferred from a selected strain of *Candida antarctica* to the host organism *Aspergillus oryzae* that produces the

enzyme. The produced enzyme is immobilized onto a macroporous acrylic resin (Product information, Novo Nordisk). The lipase is about 10 wt% of the total weight of immobilized resin.<sup>23</sup> Active site titration of immobilized CAL-B is employed in a non-aqueous solvent. It was found that 50% of Novozym 435's immobilized protein was catalytically active.<sup>24</sup>

#### 1.1.2 Enzymatic synthesis of functional polyesters

Enzymatic polyester synthesis is the versatile approach to produce polyesters. It is especially useful when there is the need to synthesize functional polyesters.<sup>25</sup> Functional polyesters are polyesters possessing pendant functionalities such as mercapto,<sup>26</sup> hydroxyl,<sup>27-29</sup> epoxy,<sup>4</sup> halides,<sup>30</sup> solketal,<sup>31</sup> azide<sup>28</sup> groups, and unsaturated entities<sup>32-36</sup> at the polymer main chain. Functional polyesters are classically synthesized by pre-modification of cyclic monomers followed by ring opening polymerization,<sup>37,38</sup> which involves several protection-deprotection steps carried out by metal-based catalysts, which are toxic and difficult to remove from the product.<sup>30</sup> Polycondensation reactions of monomers containing more than two functional groups lead to hyperbranched or cross-linked polymers.<sup>39-42</sup> Since the enzyme is regio-, enantio- and stereoselective, 43-45 this can help to synthesize chiral and optically active compounds.<sup>45</sup> These features facilitate the production of linear functional polyesters out of monomers bearing multiple functionalities. Many of them are obtained from renewable resources and difficult to polymerize using chemical catalyst. Poly(butylene succinate-co-itaconate) is the most recent example of such polymers.<sup>46</sup> Enzymatic polymerization is carried out at mild reaction condition, so this feature helps to polymerize thermally sensitive monomers.<sup>47</sup>

Many monomers derived from triglycerides are used for enzymatic polyesterification to produce polyesters.<sup>48–52</sup> High molar mass biobased polyesters up to 70,000 kDa, from ω-carboxy fatty acid such as 1,18-*cis*-9-octadecenedioic, 1,22-*cis*-9-docosenedioic, and 1,18-*cis*-9,10-epoxy-octadecanedioic acids and diols, were obtained.<sup>53</sup> Glycerol, which is a byproduct of biofuel production, was extensively used for the synthesis of functional polyesters under several reaction conditions and in the presence of lipases derived from different origins.<sup>54–57</sup> A linear polymer is obtained as the reaction occurs principally at primary hydroxyl groups of glycerol, only 5-10 mol% of secondary hydroxyl groups are reacted at 50°C.<sup>54</sup> Poly(glycerol sebacate) (PGS), and

poly(glycerol adipate) (PGA) are examples of glycerol-based polyesters.<sup>34,54,58</sup> They are also synthesized on large scale.<sup>33,59</sup>

Sometimes terpolymers are synthesized to achieve high molar mass polyesters which are based on two different types of diols<sup>56,60</sup> or diacids.<sup>60</sup> Activated diacids and their derivatives such as divinyl esters may also be used to produce polymers with high molar mass. The most common example of diester used for transesterification reactions is divinyl adipate since it is commercially available and provides an irreversible system, as the condensation side product is vinyl alcohol that tautomerizes to acetaldehyde. Acetaldehyde is a gas at room temperature that can easily leave the system, resulting in a high molar mass product.<sup>61</sup>

Like glycerol, other multihydroxy alcohols such as erythritol, xylitol, ribitol, D-glucitol, D-mannitol and galactitol obtained by reduction of sugars,<sup>52</sup> were also subjected to polymerization.<sup>62</sup> These reduced sugars are difficult to polymerize because they are only soluble in highly polar solvents such as DMF, DMSO, and pyridine. These highly polar solvents reduce the enzyme activity as it can change the enzyme confirmation.<sup>63,64</sup> Furthermore, these monomers have a high melting point, so bulk polymerization can only give a highly branched polymer.<sup>56,57,65</sup> However, sugar-based polyesters were synthesized in acetonitrile, using 60-80 wt% CAL-B with respect to total mass of monomers at 60°C.<sup>61,66</sup>

In all these polymers pendant functionalities came from alcohols. However, the pendant group could also be part of diacids, example of such diacids are malic acid, tartaric acid, fumaric acid, and glutaconic acid. Tartaric acid is highly polar and is difficult to polymerize since it deactivates the enzyme. The apparent inactivity of CALB with tartaric acid could arise from the steric demand of  $\alpha$ - and  $\beta$ -substituents. There are several reviews on enzymatic polymerizations that summarize different products obtained through enzymatic reaction.  $^{3,16}$ 

There are a plethora of factors that can affect enzymatic polymerization including temperature, pressure, water content, enzyme concentration and nature of the solvent. The selection of appropriate organic solvents is crucial as it can alter enzyme selectivity by changing the configuration of monomers. $^{68,69}$  It was found that low polarity solvents, with partition coefficients with water greater than 1.9 such as n-hexane, diphenyl ether and toluene are more suitable for enzymatic reactions. In contrast polar solvent strip off water from the active site of an enzyme called bound water necessary for

enzyme activation, hence resulting in low molar mass products due to hydrolytic cleavage of ester links.<sup>3,46,70,71</sup> The polymer conformation and radius of gyration in a solvent may alter its ability to react.<sup>13</sup>

Enzymatic esterification is a green process that could be carried out in solvent free conditions,<sup>60</sup> in ionic liquids,<sup>72</sup> and in super critical carbon dioxide (scCO<sub>2</sub>).<sup>73-76</sup> The stoichiometric ratio of DVA/diol is an important factor to generate high molar masses. The molar mass is reduced significantly when the reaction deviates from equimolarity of the functional groups.<sup>54</sup> Increasing the ratio of enzyme to substrate concentration (E/S) leads to a more rapid attainment of higher molar mass polyesters within a shorter times.<sup>71</sup>

Besides polymer synthesis, enzymes could also be used to synthesize monomers from biomass.<sup>77</sup> Another advantage of enzymatically synthesized polymers is that they can be degraded by the same enzyme that was used previously for their syntheses, hence it helps for polymer biodegradability and recycling.<sup>78–80</sup>

#### 1.1.3 Grafting of functional polyesters

The presence of functional pendant groups along the polymer backbone is a highly efficient source of tailoring the properties of polyesters including features such as hydrophilicity, biodegradation rates, and bioadhesion.<sup>81</sup>

Comb-like polyesters can be synthesized by grafting from, grafting onto and grafting through strategies. <sup>82</sup> Kalinteri *et al.* obtained amphiphilic comb-like polyesters by direct esterification of fatty acid with pendant hydroxyl groups of the polyester. Later on, they used them to prepare nanoparticle (NP) for drug delivery systems (DDS). <sup>83</sup> In another study, Orafai *et al.* have used fatty acid (caprylic and stearic acid) and amino acid (tryptophan) grafted PGA and determined the surface free energy of prepared nanoparticles from these polymers. <sup>84</sup> Zhang *et al.* have used a one-pot synthesis approach for the preparation of grafted polyesters with unsaturated fatty acids to form polymeric triglyceride analogs. <sup>85</sup> These grafted polyesters could also be cured to produce biodegradable polymeric networks. <sup>34,86</sup> Our group has extensively studied poly(glycerol adipate) grafted with saturated and unsaturated fatty acids of various lengths. It was discovered that the degree of substitution is important to attain certain morphologies of nanoparticles obtained in aqueous media. These nanoparticles were

further used as a vehicle for drug delivery systems.<sup>87,88</sup> Later on, the behavior of these amphiphilic polymers at the air/water interface was studied.<sup>89</sup>

Besides PGA, sugar-based polyesters such as poly(xylitol adipate)(PXA) and poly(D-sorbitol adipate) (PDSA) were also grafted with stearoyl chains that produce unique nanoparticles in aqueous media. 90 Grafted polymers could also be synthesized using other chemistries other than direct esterification. Thus, Naolou et al. synthesized comb-like polymers containing blocks of two crystallizable side chains i.e. poly(\varepsiloncaprolactone) and poly(ethylene oxide). They explained comprehensively the crystallization behavior of grafted copolymers.91 The phase behavior of these amphiphilic polymers at the air/water interface was also investigated.92 In another study, polyesters with azide pendant group were synthesized from polycondensation reaction of an azide group-containing diol (synthesized from 3-hydroxymethyl-3methyloxetane) and grafted with azide-alkyne click reaction using PEO to produce water-soluble polymers.<sup>28</sup> Later on, Wu et al. synthesized azido functionalized polyesters starting from 2-azido glycerol which after click reaction with PEG, produced a comb-like polymer. This comb-like polymer self-assembles in the form of spherical micelles in aqueous media, and it has a relatively low critical micelle concentration (CMC).93 Yet in another approach, grafted polyesters were obtained using chloro functionalized caprolactone. After polymerization the chloro-functionality was replaced by an azide group which after azide-alkyne click reaction, produced grafted polyesters. 94-96 In another approach polyesters with pendant acetylene groups were synthesized by azide-alkyne click reaction with azide functionlized PEG chains or oligopeptides. This produced grafted polymers that could be used for tissue engineering. 94 [beily et al. have converted hydroxyl pendant group of polyesters to macro-initiators for atom transfer radical polymerization (ATRP), that after ATRP of poly(glycerol methacrylate) (PGMA) produced a water-soluble copolymer.<sup>97,98</sup> In another approach a methacrylic backbone was synthesized by ATRP followed by eROP of ε-caprolactone to produce a grafted copolymer.<sup>76</sup> Grafting of functional polyesters can also be used to prepare biodegradable elastomers. 99 Mecerreyes et al. obtained grafted polymers by a combination of ROP and ATRP followed by the formation of polymeric networks using a Micheal type addition. 100

Functional polyesters provide an opportunity to conjugate proteins and drugs with them. In this respect Wersig *et al.* used poly(glycerol adipate) for conjugation of

indomethacin drug.<sup>101</sup> In another report Garnett and coworkers have conjugated methotrexate which is an anticancer drug to poly(glycerol adipate) and have done toxicity and degradation studies of the polymer conjugates.<sup>102</sup>

#### 1.2 FUNDAMENTALS OF LIPID SELF-ASSEMBLY

Glycerol monooleate (GMO) is a molecule composed of glycerol acylated with oleic acid (monounsaturated omega-9 fatty acid) mainly at position 1 of glycerol. The chemical structure of GMO is shown in Figure 1.1.

**Figure 1.1**. Chemical structure of glycerol monooleate (GMO).

The other two hydroxyl groups of glycerol together with the ester bond provide the polar character to this part of the molecule also called the *head* group. They can form hydrogen bonds with water molecules in aqueous medium. In contrast the oleic acid chain is hydrophobic and is usually referred as the *tail*. The resulting glycerol monooleate is an amphiphilic molecule with a hydrophilic-lipophlic balance (HLB) value of 3.8 as determined by Griffin's method. GMO is also referred to as magic lipid as it shows a rich mesomorphic behavior. Lipids self-assemble into different liquid crystalline structures under varying conditions of temperature (thermotropic phases), 105,106 pressure (barotropic phases), 105,109 and by the addition of a third component. 110–115

One of the major driving forces for different self-assemblies of lipids in water is the hydrophobic effect, (which acts to minimize the interface between the hydrocarbon tails of the amphiphile and the aqueous environment) together with others interactions, including van der Waals interactions and head group hydrogen bonding. The self-assembling process driven by these forces is spontaneous, i.e. for this process the value of Gibbs free energy of aggregation (Equation 1.1) is negative.

$$\Delta G_{agg} = \Delta H_{agg} - T \Delta S_{agg}$$
 1.1

Here  $\Delta S_{agg}$  is the change in entropy of aggregation and  $\Delta H_{agg}$  is the change in enthalpy of aggregation. A direct relationship between Gibbs free energy of aggregation and critical aggregation concentration is given by:

$$\Delta G_{aaa} = RT ln(CAC)$$
 1.2

where R is universal gas constant and T is the absolute temperature. The several factors which determine or affect the formation of particular structures. The concentration, temperature and shape of an amphiphile play a decisive role. Polymers form micelles when the concentration is equal to or greater than the critical micelle concentration (CMC), and when the temperature is greater than the critical micelle temperature (CMT), also known as the Kraft temperature. Besides micelles, several other self-assemblies are also possible. The fundamental principle behind different self-assemblies of amphiphilic molecules is their shape. The shape of the molecule can be described qualitatively according to the theory by Israelachvili. This theory is based on the dimensionless packing parameter  $\gamma$ , also called the critical packing parameter or shape factor.

$$\gamma = \frac{v_l}{a_0 l_c} \tag{1.3}$$

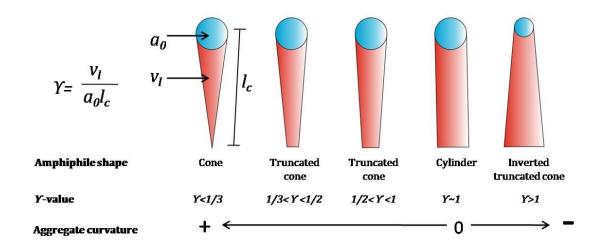
Where  $l_c$  is the length of hydrophobic chain of lipid,  $a_0$  is the effective amphiphile head group area, and  $v_l$  is the average volume occupied by an amphiphilic molecule. The hydrocarbon chain length and volume for simple, single chained amphiphiles may be evaluated by the empirical formula.<sup>122</sup>

$$v_l = (27.4 + 26.9n_c) \,\text{Å}^3$$
 1.4

$$l_c = (1.5 + 1.26n_c) \text{ Å}$$
 1.5

Here,  $n_c$  is the number of carbon atoms. The shape factor  $\gamma$  describes the local packing constraint and allows amphiphiles to be categorized by their shape (see Figure 1.2).  $\gamma>1$  gives  $type\ 2$  or inverse self-assembly (curvature towards the water regions) e.g. wedge shape molecules like MAG (monoacylated glycerol) and block copolymers having a relatively more hydrophobic character and small head groups.  $\gamma<1$  shows  $type\ 1$  or normal self-assembly (curvature towards the chain region). Molecules with the larger head group,  $\gamma=1$  (flat bilayer with nearly zero curvature) e.g. cylindrical shape molecule shows lamellar morphology. In case of GMO, the cis double bond at the

9,10-position makes the hydrocarbon tail sterically demanding, thus triggering the formation of inverse or *type 2* micelles with  $\gamma > 1$ .



**Figure 1.2:** The critical packing parameter  $\gamma$  of amphiphiles and the related aggregate curvature (Figure is modified from literature.<sup>124</sup>).

In addition to  $\gamma$ , degree of hydration of amphiphilic molecule is an important factor that leads to different self-assemblies. Most common self-assemblies are lamellar, hexagonal and bicontinuous cubic phases. Additional phases are formed, usually by the incorporation of other components and/or energy. Due to their dimensional arrangement in the nanometer range and solid-liquid mediation, the lipid polymorphs are also called liquid crystalline nanostructures.

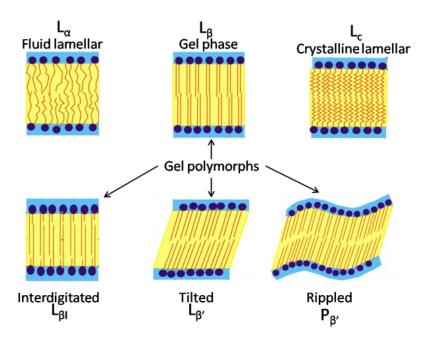
#### 1.2.1 Lipid polymorphism

#### 1.2.1.1 The lamellar phase

The lamellar phase consists of a lipid bilayer stacked on each other separated by a water layer. Three main types of lamellar phase have been given in the literature, 125 crystalline lamellar  $L_c$ , fluid lamellar  $L_\alpha$  and lamellar gel  $L_\beta$  phases. The lamellar phase is characterized by SAXS peaks which appear in the ratio 1:2:3:4..... Different types of lamellar phases could be distinguished from each other by comparing their characteristic WAXS pattern. In the  $L_c$  phase, molecules are ordered into a fixed position. It shows much intense Bragg reflections. The fluid lamellar  $L_\alpha$  phase is a true liquid crystalline phase. In this phase, the head groups are completely disordered and the hydrocarbon chains are fluid like. It shows a diffuse scattering in the wide angle region, typically at 4.5 Å while the lamellar gel  $L_\beta$  phase is formed at high temperatures.

In this phase the hydrocarbon chains are arranged parallel to the layer normal. Some other lamellar phases could also be observed. These are the tilted gel  $L_{\beta'}$  phase, the interdigitated gel  $L_{\beta l}$  phase, and the rippled gel  $P_{\beta'}$  phase.

The tilted gel  $L_{\beta'}$  is a tilted version of the  $L_{\beta}$  phase, and different tilt directions with respect to the underlying hexagonal lattice may occur. The tilting occurs when the head group packing requirement is exceeded. Above a certain excess of tilting the packing is stabilized by inter-digitation of the chains (without tilting) allowing head groups to pack in twice the area than that of the normal gel phase. This is called the interdigitated gel phase  $L_{\beta l}$ . The lamella of  $L_{\beta'}$  phase may undergo periodic modulation which results in a rippled phase  $P_{\beta'}$ , observed at high temperatures just below the fluid lamellar phase  $L_{\alpha}$ . Schematic description of all lamellar phases is shown in Figure 1.3.



**Figure 1.3.** Commonly observed crystalline and liquid crystalline lamellar phases observed in lipids. Figure modified from Kulkarni  $et\ al.^{123}$ 

The lattice parameter for lamellar phases can be calculated from the corresponding reciprocal spacing,  $s_{lam} = (n/a_{lam})$ , where n is the order of the reflection (1, 2, 3, 4,.....),  $a_{lam}$  or d is equal to the lattice parameter of the lamellar phase, i.e. the distance between the repeat unit. In the lamellar phase, the monolayer thickness can be determined using the relation,  $d_l = 0.5(a_{lam} - d_w)$  where  $d_w$  is the water layer thickness which is  $\phi_w d$  (here  $\phi_w$  represents water volume fraction).

#### 1.2.1.2 The hexagonal phase

The hexagonal phase is comprised of a group of micellar cylinders onto a 2-D hexagonal lattice.<sup>128</sup> The hexagonal phase may be 'normal'  $H_1$  or 'reverse'  $H_2$ . The normal hexagonal phase has a curvature towards the hydrocarbon chain region of the lipid, in contrast, the reverse hexagonal phase displays a mean curvature towards the aqueous interior. The schematic diagram of the reversed hexagonal  $H_2$  phase is shown in Figure 1.4(a). The hexagonal phase is distinguished by SAXS peaks in the ratio of  $1:\sqrt{3}:\sqrt{4}$  ....

For the hexagonal phase, the lattice parameter  $a_{hex}$  is calculated from the following relation.

$$a_{hex} = \frac{4\pi\sqrt{h^2 + k^2 + hk}}{\sqrt{3}a}$$
 1.6

The diameter of the water cylinder is given by:

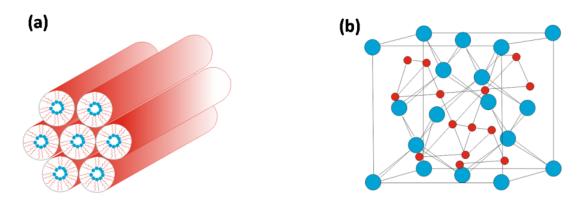
$$d_w = \sqrt{\frac{2\sqrt{3}}{\pi}(1 - \phi_l)\alpha_{hex}^2}$$
 1.7

Where,  $\phi_l$  is the volume fraction of lipid.

#### 1.2.1.3 The micellar cubic phase

The micellar cubic phase is formed by complex packing of reverse micelles on a cubic lattice that has curvatures larger than the reversed hexagonal phase. The micellar cubic phase has a Fd3m symmetry. The formation of the micellar cubic phase requires a minimum of two types of amphiphilic molecules, one of which is more strongly polar (e.g. GMO and diacyl phosphatidyl choline (PC)) and the other is weakly polar (e.g. fatty acid (FA) and diacyl glycerol). The incorporation of a weak amphiphilic compound reduces the effective hydrophilicity of the lipid head group region. This dehydration of the head group tends to drive the phase equilibrium towards the inverse phases with increasing interfacial mean curvature. The structure is discontinuous and made up of two populations of reversed micelles. (see Figure 1.4(b)). Per unit cell of the Fd3m cubic phase, there are eight larger inverse micelles, arranged tetrahedrally on a diamond lattice and sixteen small inverse micelles. To explain the existence of two types of micelles, it is assumed that the amphiphle composition is probably inhomogeneous between two types of micelles. To

could be the reason why the Fd3m cubic phase usually does not appear in lipid/water binary systems. GMO does not show this phase in pure water, but with the addition of other components to it, e.g. oleic acid or poly(ethylene imine) (PEI).<sup>110,131</sup> The Fd3m phase shows a characteristic pattern in the SAXS traces with the peak ratio,  $\sqrt{3}$ ,  $\sqrt{8}$ ,  $\sqrt{11}$ ,  $\sqrt{12}$ ,  $\sqrt{16}$  .... <sup>104</sup>



**Figure 1.4.** Schematic structure of (a) the reverse hexagonal phase  $(H_2)$ , (b) the cubic phase Fd3m. The structure consists of eight larger inverse micelles (polar cores in blue colour) and 16 smaller inverse micelles (polar cores in red colour). The remaining volume is filled by the fluid hydrocarbon chains and water (Figures are modified from literature<sup>130</sup>).

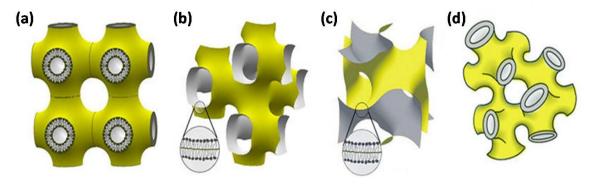
#### 1.2.1.4 Bicontinuous phases

#### **1.1.1.1.1** The sponge phase

The sponge phase  $L_3$  is a bicontinuous phase found in several amphiphiles. This phase has a bicontinuous sponge-like structure with a lipid bilayer separating the polar solvent space into two disconnected volumes, similar to bicontinuous cubic phases. The only difference is that they do not possess long-range order and their structure can be considered as a melted cubic phase. In the phase diagrams,  $L_3$ -phases occupy regions adjacent to lamellar phases and both reversed as well as normal type sponge phases are possible. It is identified by a broad peak in the SAXS region. The GMO-water system itself does not show this phase unless a third component such as low molar mass PEG or salt Is added.

#### 1.1.1.1.2 Bicontinuous cubic phases

In the last couple of decades, there is an exponential increase in the use of bicontinuous cubic phases in drug delivery system<sup>138–140</sup> and in membrane protein crystallization.<sup>141</sup> Bicontinuous cubic phases have an intermediate curvature between a flat lamellar phase and a cylindrical hexagonal phase. These phases are described on the basis of infinite periodic minimal surfaces (IPMS).<sup>142</sup> IPMS have zero mean curvature *H* and negative Gaussian curvature *K*. They consist of parallel curved bilayers, forming a complex network with 3-D cubic symmetry, which separates two continuous but non-intersecting water channels.<sup>143</sup> Schwarz, for the first time, introduced mathematically, double diamond and primitive surfaces.<sup>142,144</sup> Later, a closely related structure known as gyroid was introduced by Schoen.<sup>145</sup> The cubic phases are characterized by their crystallographic space groups having *Im3m* (primitive), *Pn3m* (double diamond), and *Ia3d* (gyroid) symmetry identified by corresponding space group numbers 229, 224 and 230.<sup>122</sup> Schematic diagrams of all bicontinuous cubic phases are shown in Figure 1.5.



**Figure 1.5.** Bicontinuous phases formed by lipids. (a) Bicontinuous cubic phase Im3m ( $Q^{P_2}$ ,  $Q_{229}$ ), (b) bicontinuous cubic phase Pn3m ( $Q^{D_2}$ ,  $Q_{224}$ ), (c) bicontinuous cubic Ia3d ( $Q^{G_2}$ ,  $Q_{230}$ ), and (d) sponge phase (Figure is adapted from Koynova *et al.*<sup>146</sup>).

The inverse bicontinuous cubic phase of *type 2* consists of a single continuous lipid bilayer wrapped on a minimal surface on either side of which lies a continuous region of water. In the Im3m phase, water channels meet at 90° in 6-way junctions and in the Pn3m phase in 4-way junctions at 109.5°. In the Ia3d phase, water channels meet in 3-way junctions at 120°. Due to the cubic symmetry, they are isotropic, hence appear dark when viewed through a polarized light microscope.  $^{104,109,122}$ 

The most common way to identify these phases is by their SAXS pattern where the scattering vector q of the Bragg peaks is given by

$$q = \frac{2\pi\sqrt{h^2 + k^2 + l^2}}{a_{cubic}}$$
 1.8

where, h, k and l are Miller indices of the Bragg peak, and  $a_{cubic}$  is the lattice parameter of the cubic phase. The individual type of the cubic phase is identified by the characteristic ratios as  $3m:\sqrt{2},\ \sqrt{4},\ \sqrt{6},\ \sqrt{8},\ \sqrt{10},\ \sqrt{12},\ \sqrt{14},\ \sqrt{16},\ \sqrt{18}$ , Pn3m: $\sqrt{2},\ \sqrt{3},\ \sqrt{4},\ \sqrt{6},\ \sqrt{8},\sqrt{9},\ \sqrt{10},\ \sqrt{11}$  ..., and  $la3d:\sqrt{6},\ \sqrt{8},\ \sqrt{14},\ \sqrt{16},\ \sqrt{20},\ \sqrt{22},\ \sqrt{24},\ \sqrt{26}$ .....

The monolayer thickness or lipid chain length  $l_c$  of the cubic phases is determined by solving the equation  $1.9.^{142,147}$ 

$$\Phi_{lipid} = 2\sigma \left(\frac{l_c}{a_{cubic}}\right) + \frac{4}{3}\pi \chi \left(\frac{l_c}{a_{cubic}}\right)^3$$
 1.9

Where  $l_c$  is lipid chain length/monolayer thickness,  $a_{cubic}$  is the lattice parameter of the corresponding phase,  $\chi$  is the Euler-Poincare characteristics. The lipid length throughout the unit cell of such cubic phases can be assumed to be constant. The interfacial area integrated over a single monolayer is given by equation  $1.10.^{142}$ 

$$A_l = \sigma a_{cubic}^2 + 2\pi \chi l_c^2$$
 1.10

 $\sigma$  is a unitless quantity that describes the ratio of the area of the minimal surface in a unit cell to the (unit cell volume)<sup>2/3</sup>. The space group of the cubic phase determines the type of IPMS associated with the cubic phase and thus, the values of  $\sigma$  and  $\chi$  are calculated (see Table 1.1).

**Table 1.1.** The Euler-Poincare characteristic  $\chi$  and the surface area of the minimal surface per unit volume  $\sigma$  for different types of infinite periodic minimal surface.<sup>122</sup>

Space group	Space group number*	IPMS Type	χ**	σ**
Pn3m	224	D(Diamond)	-2	1.919
Im3m	229	P(Primitive)	-4	2.345
Ia3d	230	G(Gyroid)	-8	3.091

<sup>\*</sup>Number corresponds to the space group of the cubic lattice.\*\* Type refers to common names used to identify particular IPMS.<sup>142</sup>

The cross-sectional area per lipid molecule at a distance l from the minimal surface is given by  $^{148}$ 

$$A_{cs}(l) = \frac{2A(l) \cdot v_{lipid}}{\phi_{lipid} \cdot a_{cubic}^3}$$
 1.11

where,  $v_{lipid}$  and  $\phi_{lipid}$  are the molecular volume and the volume fraction of the lipid, respectively. By assuming a lipid-specific volume  $\tilde{v}$  of 1 cm<sup>3</sup>·g<sup>-1</sup> (10<sup>24</sup> Å<sup>3</sup>·g<sup>-1</sup>),  $v_{lipid}$  is calculated as

$$v_{lipid} = \frac{M\tilde{v}_{lipid}}{N_A}$$
 1.12

Where, M is the molar mass of lipid and  $N_A$  is the Avogadro's number. For GMO the value of  $v_{lipid}$  is 593 Å<sup>3</sup>/molecule. The number of lipid molecules in the unit cell of the cubic phase  $n_{lipid}$  is given by

$$n_{lipid} = \frac{\phi_{lipid} \cdot a_{cubic}^3}{v_{lipid}}$$
 1.13

The radius of the water channel  $r_w$  is calculated based on minimal surfaces 147

$$r_w = \left(-\frac{\sigma}{2\pi\chi}\right)^{1/2} a_{cubic} - l_c$$
 1.14

Putting values of  $\sigma$  and  $\chi$  for corresponding cubic phases from Table 1.1, the equation takes the following form, for the Pn3m phase:  $r_w = 0.391a_{cubic} - l_c$ , for the Ia3d phase  $r_w = 0.248a_{cubic} - l_c$ , for Im3m phase:  $r_w = 0.306a_{cubic} - l_c$ .

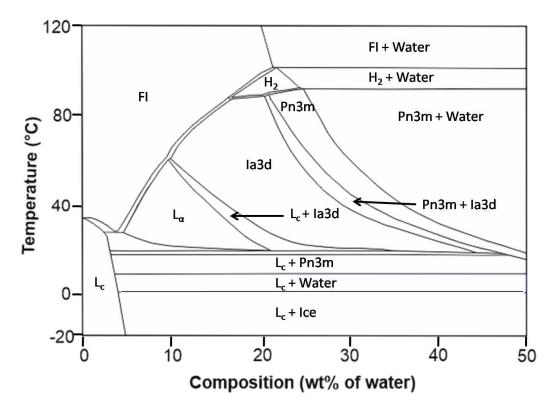
#### 1.2.2 Binary phase diagram of GMO-water system

To understand the GMO-water polymorphism, the temperature-GMO content in water phase diagram was established by Lutton. He used polarized optical microscopy to identify different phases. He has found lamellar, hexagonal and cubic phases as neat, middle, and viscous isotropic phase, respectively. His phase diagram could not help much as all the cubic phases appear black under polarized optical microscopy, hence one cannot distinguish between different cubic phases. Then, great efforts have been made to explore the equilibrium phase behavior of GMO in water. In this regards, several authors have contributed to identify various phases and explained their structure. He was a structure of the equilibrium phase behavior of the equilibrium phase and explained their structure.

Hyde *et al*. presented a complete phase diagram with the help of polarized optical microscopy and X-ray diffraction. <sup>154</sup> The phase behavior was studied for a temperature

range of 20-110°C and for a hydration of 0 to 40 wt%. They identified a different region in the phase diagram labeled with different phases such as fluid lamellar  $L_{\alpha}$ , cubic Ia3d, cubic Pn3m, reverse hexagonal  $H_2$  and fluid isotropic  $L_2$  phases quite clearly along with mixed phase regions. Caffery and co-worker have extensively studied the mesophase behavior of several monoacyl glycerols (MAGs) including GMO and determined the structure parameter of the GMO-water system. Briggs  $et\ al$  explained the equilibrium phase behavior for a temperature range from 0 to 104°C and for the hydration level from 0 to 47 wt% in steps of 5°C and average 2 wt% water respectively. The phase region is quite similar as was observed by Hyde  $et\ al$ , however, they ensured that all the observed phases are in equilibrium.

Later, Qui *et al.* described the metastable phase regions (below 20°C) in their phase diagram.<sup>121</sup> Combining the low-temperature region with that of the earlier phase diagram, the new phase diagram was merged which is shown in Figure 1.6. In Figure 1.6 the low-temperature part of the phase diagram is included, showing a crystalline phase *Pn3m* along with water and ice.



**Figure. 1.6.** Composition phase diagram of the GMO-water system that combines the phase diagram of Briggs *et al.* and that of Qiu and Caffery. (Figure is modified from Qiu *et al.* 106)

At low temperature and low water content, a lamellar crystalline region  $L_c$  exists that contains more than one polymorph. The  $L_c$  phase was identified in dry samples

and the polymorphism found in this region was not investigated in detail. At low water content, the  $L_c$  phase melts with increasing temperature into a fluid isotropic phase FI, which is also known as inverse micellar phase  $L_2$ .<sup>154</sup>

With increasing water content, a phase transition from the crystal lamellar  $L_c$  phase into the lamellar liquid crystalline phase  $L_\alpha$  takes place. With increasing temperature, the  $L_\alpha$  phase melts again into the fluid isotropic FI phase. With further increasing water content, the bicontinuous cubic phases are formed with two different space groups, Ia3d, and Pn3m. For composition with water contents of 17 wt% or more, with increasing temperature, a phase transition from the bicontinuous cubic phase into an inverse hexagonal phase  $H_2$  and finally into the isotropic FI phase takes place. Above a certain amount of water, phase separation occurs into a structured phase and an excess water phase indicating the maximum water carrying capacity of the individual phase. It is noteworthy that the bicontinuous cubic Pn3m phase can carry more water (~40 wt%) than the  $H_2$  (~25 wt%) or the FI phase (~20 wt%). Excess-water phase separation allows dispersing the respective structured phase into water called a nanostructured emulsion. A more detailed discussion about the dispersion of submicron cubic particles (cubosomes) and their stabilization will be given later in this chapter.

# 1.2.3 The effect of additives on the mesophase behavior of the GMO-water system

The liquid crystalline phases of the GMO-water system can tolerate a specific amount of a third component. A further addition to the system results in swelling or shrinkage of water channels and ultimately to phase transitions. Misquitta and Caffrey have done a detailed study on the effect of detergent on the mesophase behavior of the GMO-water system. They observed a phase transition from Pn3m to the lamellar  $L\alpha$  phase via~la3d when n-alkyl-b-D-glucopyranosides were added. Sodium chloride (NaCl) or sodium sulphate (Na<sub>2</sub>SO<sub>4</sub>) are well-known kosmotropes which show strong hydration behaviour resulting in the dehydration of the GMO head groups. This results in a decrease in occupied surface area of lipid head group and hence the radius of the water channel decreases and so the lattice parameter. On the contrary, a chaotropic electrolyte such as sodium iodide (NaI), sodium thiocyanate (NaSCN), potassium thiocyanate (KSCN), and urea leads to an increase in the hydration of the

monoolein head group resulting in an increase of the radius of the water channel and hence the lattice parameter.  $^{136,160}$  Sugars also act as kosmotropes and induce a phase transition from Ia3d to  $H_2$  via Pn3m. Some cryoprotectants such as glycerol and DMSO also affect the GMO-water phase behavior. Glycerol (being kosmotropic), when added to hydrated GMO, decreases the lattice parameter of the cubic phase and reduces the cubic phase region. On the other hand, DMSO (being chaotropic) increases the Pn3m and Im3m coexistence regions and also increases the lattice parameter of cubic phases.  $^{136,161}$ 

The effect of several biomacromolecules, especially soluble proteins, on the mesophase behavior of the GMO-water system has also been studied. The protein-GMO-water phase diagram was constructed for lysozyme. It shows all three bicontinuous cubic phases. 162–165

The effect of several amphiphiles having different degrees of unsaturation and hydrocarbon chain lengths on the lipid cubic mesomorphism was also investigated. It was observed that all single chain amphiphiles having  $\gamma \ge 1$  results in a phase transition from cubic Ia3d to the more negatively curved hexagonal  $H_2$  phase and ultimately to the  $L_2$  phase.<sup>109,122</sup> In some cases, the micellar cubic Fd3m phase can be observed between the  $H_2$  and  $L_2$  phases. <sup>109</sup>

For many molecules, a phase transition from the cubic Pn3m to the  $L_{\alpha}$  phase occurs via the cubic Im3m and cubic Ia3d phase. This transition is due to the addition of an amphiphile with  $\gamma<1$  which leads to less negatively curved phases than the cubic phase. Cubosomes are an effective vehicle for drug delivery system. Incorporation of hydrophobic drugs induce a phase transition from cubic Pn3m to negatively curved  $H_2$  and FI phases. The hydrophobic character relieves packing frustration of the alkyl chains.  $^{166}$ 

Cubic phases are a good source for *in meso* crystallization of membrane proteins. The effect of poly(ethylene glycol) (PEG) of various chain lengths on the cubic phase of the GMO/water system are studied for the purpose of crystallization of proteins.  $^{141,167}$  It is reported that a low molar mass PEG such as PEG400 induces a phase transition from cubic Pn3m to the FI phase of the GMO/water system, while PEG1000 does not induce the phase transition of the cubic Pn3m phase of the GMO/water system. However, PEG with higher molar masses (3,500-20,000 g·mol-1) induces a phase

transition of cubic Pn3m to the  $L_{\alpha}$  phase as a consequence of osmotic pressure that results in dehydration of the cubic phase.

Kumar *et al.* presented a detailed investigation of the phase behavior of the glycerol monooleate-water-PEI system. According to them, the GMO-water systems containing small fractions (2-4 wt%) of low molecular weight PEI form an ordered reverse micellar cubic phase with Fd3m symmetry. For higher molar mass (25 kDa), the Fd3m phase is formed at 4 wt% PEI, in coexistence with the fluid isotropic FI phase.<sup>110</sup>

For all solvents and soluble additives, the tendency to interact with the polar-apolar interface was found to be important. The insertion of the soluble additives into the head group region was found to lead to the formation of the less negatively curved  $L_{\alpha}$  phase due to a decrease in the  $\gamma$ -value with increasing head group volume ( $\gamma$  >1 to ~1). This was observed for solvents, strong chaotropic salts, short peptides that interact with the lipid membrane, block copolymers with a relatively large amount of PPO blocks, and a few hydrophilic small molecules. Several additives such as block polymers and PEGylated lipids etc. are used to stabilize submicron particle dispersions of the cubic phase (cubosomes). The details of steric stabilizers used for cubosome dispersions are given in the following section.

#### 1.3 STERIC STABILIZERS FOR CUBOSMES

As discussed before, the bulk cubic phase can be dispersed in water into submicron particles. Submicron particles of bulk cubic phases are called cubosomes. These have gained huge interest for their use as drug delivery vehicle and *in meso* crystallization of membrane proteins. <sup>138,141,168,169</sup> Cubosome dispersions are obtained by two approaches (a) top-down (dispersing the bulk cubic phase using high energy), and (b) bottom-up (dispersing the lipid in water after dissolving it in an organic solvent). <sup>170</sup> Cubosomes are sterically less stable because of weak van der Waals forces which cannot prevent coalescence. Therefore, a steric stabilizer is always required for the stability of cubosomes. An ideal stabilizer prevents flocculation without disrupting the inner cubic structure. The structure and concentration of stabilizers are two important factors responsible for the stability of a dispersion. <sup>171</sup>

Most commonly used polymers as steric stabilizers are triblock copolymers consisting a PPO block sandwiched between two PEO blocks. These are known as

Poloxamer<sup>™</sup> or Pluronics<sup>®</sup>. Among pluronics, Pluronic<sup>®</sup>F127 is the most employed steric stabilizer (see Figure 1.7 for the structure). It consists of a middle block of PPO of 65 monomer units and two blocks of PEO of 100 monomer units to both sides of PPO (PEO<sub>100</sub>-PPO<sub>65</sub>-PEO<sub>100</sub>) having a molar mass of 12,600 g·mol<sup>-1</sup>. The PPO block serves as an anchor while the PEO blocks in the water channels or spread outside to provide steric shielding.<sup>172,173</sup>

Figure 1.7. Chemical structure

of some pluronics.

Pluronic® has been employed to several cubosome dispersions, including GMO, glycerol monolinoleate and phytantriol. Among these, GMO was most extensively studied. For a low concentration of Pluronic®F127 (<4 wt% with respect to GMO) cubosomes with *Pn3m* symmetry, and for a higher concentration of Pluronic®F127 (10 wt% with respect to GMO), cubosomes with Im3m symmetry are produced.<sup>131,174</sup> It is important that *Pn3m* symmetry of cubosomes should remain as the change to *Im3m* space group symmetry indicates destabilization of the *Pn3m* cubic symmetry which results in fast drug release. <sup>175</sup>

However, the *Pn3m* cubic phase of glycerol monolinoleate<sup>176</sup> or phytantriol<sup>177</sup> retained its symmetry even at high concentration of Pluronic<sup>®</sup>F127. Besides Pluronic<sup>®</sup>F127, other pluronics could also be used as steric stabilizers. Chong *et al.* have done a comprehensive investigation on a series of pluronics and conclude that Pluronic<sup>®</sup>F108 has shown a better stabilization effect for cubosomes than Pluronic<sup>®</sup>F127.<sup>178,179</sup> Pluronic<sup>®</sup>F108 has longer PEG chains compared to Pluronic<sup>®</sup>F127. It has the structure PEG<sub>132</sub>PPO<sub>50</sub>PEG<sub>132</sub> and has a molar mass of 14,600 g·mol<sup>-1</sup>. After these findings, researchers had frequently used Pluronics<sup>®</sup>F108 for stabilizing drug loaded cubosomes.<sup>180,181</sup> Several other low molar mass pluronics such as F68, P104, P105 were also used.<sup>178,182</sup>

Several lipids, after making them water-soluble by attaching PEG chains are also reported as steric stabilizers for cubosomes, e.g. GMO connected with a short PEG chain (MO-PEG660)<sup>183</sup> or a long PEG chain containing monoolein (MO-PEG2000).<sup>184</sup> In addition, PEGylated phospholipids were also used as a steric stabilizer. These include **PEGylated** 1,2-dioleoyl-*sn*-glycerol-3-phosphoethanolamine (DOPE-PEG2000), PEGylated 1,2-distearoyl-sn-glycerol-3-phosphoethanolamine (DSPE-PEG2000), and 1,2-dimyristoyl-*sn*-glycerol-3-phosphoethanolamine (DMPE-PEG550). PEGylated They produce cubosomes with *Im3m* symmetry. 185-187 Furthermore, the polysorbate series (Tween® 20, 40, 60, 80) was also studied to investigate their ability of steric stabilization of cubosomes and it was observed that only Tween® 20 and 80, commonly known as polysorbate 20 and polysorbate 80 are better stabilizers compared to other compounds of this series. 182,188 Chong et al. used PEG-stearates (Myrj-series) to stabilize cubosomes from phytantriol in aqueous media. Among all explored PEG-stearates, i.e. PEG-stearates with 10, 20, 25, 40, 45, 50, 55, 100 and 150 PEG units, it was claimed that only those PEG-stearates are able to form aqueous dispersions of cubosomes that have 40 or more PEG repeating units. Those with PEG unit greater than 100 were able to retain the *Pn3m* symmetry. 179,189

Grafted polymers were also employed to stabilize cubosome dispersions. Chong *et al.* synthesized grafted copolymers of phytantriol and PEG of various chain lengths. They observed that copolymers with HLB>17 are better stabilizers.<sup>190</sup> In another study, Chong *et al.* synthesized copolymers of poly(octadecyl acrylate)-*block*-poly(polyethylene glycol methyl ether acrylate) (P(ODA)-*b*-P(PEGA-OMe)) by RAFT polymerization. They found that increasing the PEG density in the copolymer leads to better stabilization compared to the linear block copolymer Pluronic®F127. Using this copolymer, they obtained cubosomes with *Im3m* and *Pn3m* symmetries for GMO and phytantriol, respectively.<sup>111</sup>

#### 1.4 AIMS AND OBJECTIVES

As mentioned before in this chapter, enzymatic synthesis of polyesters using CAL-B is a green process, which allows synthesis of polyesters from bio-based building blocks with numerous functionalities. Functional polyesters support the tailoring of polymers with desired properties for conjugation of drugs and proteins. Polymers grafted with hydrophobic side chains (saturated fatty acids of various chain lengths)

result in amphiphilic polymers. The self-assembling behavior of amphiphilic polymers in aqueous media results in diverse morphologies depending on the respective fatty acid and the degree of grafting. The first aim of this work is to produce functional polyesters by enzymatic transesterification reaction of divinyl adipate and multihydroxy alcohols such as sugars (D-sorbitol or xylitol) using CAL-B. These functional polyester backbones are then grafted with stearic acid to obtain amphiphilic comb like polymers. Properties of these polymers in bulk and their aqueous dispersions are analyzed to investigate their self-assembling behavior. The second objective of this work is to synthesize poly(glycerol adipate) and oleate grafted PGAs with various degrees of grafting, and to study the bulk properties of these polymers by <sup>1</sup>H NMR spectroscopy, GPC, DSC, and XRD. Another objective is to study the effect of the mesophase behavior of the GMO-water system after adding graft copolymers. As the unsaturated fatty acids grafted chains in the polymer and in the GMO are identical, they could interact with each other affecting its mesophasic behavior. For this purpose PGA*g*-022 is chosen as it has a comparable volume fraction of hydrophobic side chains with that of GMO.

The final aim of this work is to make oleate grafted poly(glycerol adipate) (PGA-g-Ox) water soluble by grafting a water soluble polymer to the polymer backbone. Poly(ethylene glycol) is a good choice for this purpose as it is a neutral, water-soluble polymer with extraordinary biological properties, which makes it suitable for various applications, including drug delivery, cell encapsulation, and conjugation to biomacromolecules.<sup>191</sup> Poly(glycerol adipate) is prepared with different degrees of grafting of oleate chains and low molar mass PEG chains such as PEG750 and PEG1K in order to achieve different degrees of hydrophilicity. The bulk properties of the synthesized graft copolymers are studied using <sup>1</sup>H NMR spectroscopy, GPC, DSC, SAXS, and WAXS. Since amphiphilic graft copolymers have a lower critical aggregation concentration (CAC) than linear block copolymers, the ability of these multigraft copolymers to stabilize the cubosome dispersions are investigated using tensiometry (to find CAC), SAXS (to find the internal structure of cubosomes) and DLS measurements (to find the particle size of structured nanoparticles)

.

### **Chapter 2**

#### 2 FATTY ACID MODIFIED SUGAR BASED POLYESTERS

#### 2.1 INTRODUCTION

Aliphatic functional polyesters are an important class of materials for pharmaceutical and biological applications because of their biocompatibility and biodegradability.<sup>192</sup> The enzymatic synthesis of functional polyesters is an attractive alternative to classical polycondensation or ring opening polymerization, which require an extensive protection and deprotection chemistry for the introduction of functional groups to the polyester backbone.<sup>37</sup> The most frequently used enzyme for polycondensation is lipase B from Candida antarctica (CAL-B) which is commercially available immobilized on acrylic resins. 193 Since CAL-B supports the esterification of primary OH-groups rather than secondary OH-groups at reasonably low temperatures, it is frequently employed to prepare linear polyesters from polyols as glycerol or sugars. 54,61,83,194,195 As second reactants usually divinyl esters, 83,196 or dimethyl esters<sup>54,195,197</sup> are employed. A typical polyester with a pendant OH-group in every monomer unit is poly(glycerol adipate) (PGA) obtained by reacting glycerol with divinyl adipate.83 We have extensively studied PGA grafted with several fatty acids. Selfassembled nanoparticles obtained from these amphiphilic polymers have been studied for drug delivery applications.<sup>87</sup> Different shapes of nanoparticles could be produced in water by the interfacial deposition method depending on the degree of substitution and on the fatty acid used. Important for the structure formation of the nanoparticles is the phase separation between polymer backbone and side chains.<sup>87,88</sup> Saturated fatty acids with relatively long acyl chains (>C12) tend to crystallize after phase separation whereas unsaturated fatty acids as e.g., oleic acid lead to the formation of two disordered nanophases. The PGA backbone obtained by enzymatic polymerization is hydrophilic but not water soluble and has usually M<sub>n</sub>-values below 10,000 g⋅mol<sup>-1</sup>. It should be mentioned here that higher molar masses can be achieved at higher polymerization temperatures but then the selectivity between primary and secondary OH-groups is partially lost.<sup>65</sup> Grafting poly(ethylene oxide) (PEO) chains onto the PGA backbone results in watersoluble polymers.<sup>28</sup> When a block copolymer of PEO and poly(ε-caprolactone) is grafted

to the polymer backbone, worm-like micelles can be produced.<sup>198</sup> The PGA backbone can also be converted into an ATRP macroinitiator, which leads to a plethora of possible polymer architectures.<sup>29,98</sup>

Here, we report on the enzymatic syntheses of poly(D-sorbitol adipate) (PDSA) and poly(xylitol adipate) (PXA). Both hydrophilic polyester backbones were modified by grafting with stearic acid chloride which yields amphiphilic polymers (PDSA-*g*-S and PXA-*g*-S). All polymers are characterized by SEC and <sup>1</sup>H NMR spectroscopy. The bulk morphology of the polymers is studied by DSC, WAXS, and SAXS. Furthermore, nanoparticles are prepared from some selected polymers and characterized by DLS and TEM. Scheme 2.1 describes the syntheses of the polymers under investigation.

**Scheme 2.1.** Synthetic route to stearoyl grafted poly(xylitol adipate) (PXA-*g*-S) and poly(D-sorbitol adipate) (PDSA-*g*-S).

#### 2.2 EXPERIMENTAL PART

#### 2.2.1 Materials

Lipase N435 derived from *Candida antarctica* (CAL-B) immobilized on acrylic resin (Sigma-Aldrich Chemie GmbH, weinheim, Germany) was dried over P<sub>2</sub>O<sub>5</sub> for 24 h prior to use. N, N-dimethylformamide (anhydrous, 99.8%), acetonitrile (anhydrous, 99.8%), tetrahydrofuran (anhydrous, 99.9%), xylitol (99%), D-sorbitol (98%), stearoyl chloride (90%) and triethylamine were purchased from Sigma-Aldrich. Divinyl adipate (96%) was purchased from TCI GmbH (Eschborn, Germany). All chemicals were used without further purification. All other chemicals used in various stages like, diethyl ether, *n*-hexane, methanol, and dichloromethane were purchased from Carl Roth (Karlsruhe, Germany).

#### 2.2.2 Syntheses

#### 2.2.2.1 Synthesis of poly(xylitol adipate)

Analogous to previously published methods, poly(xylitol adipate) (PXA) can be synthesized in a single step. $^{61,66}$  Xylitol and divinyl adipate were used in a molar stoichiometric ratio of 1:1 in the presence of lipase N435. A weighed amount of xylitol (10 g, 65.8 mmol) and divinyl adipate (13 g, 65.8 mmol) were charged into the reaction flask. Afterward, 40 mL of acetonitrile was added. The solution was stirred for 30 min at 50 °C to equilibrate the temperature. The reaction was started by adding CAL-B (2.3 g, 10 wt% of total mass of monomer). After 92 h the reaction mixture was diluted by addition of an excess of DMF and the enzyme was removed by filtration. The synthesis process is described in Scheme 2.1. The filtrate was collected and the crude product was precipitated twice in diethyl ether.  $^{1}$ H NMR spectroscopy was used to confirm the purity of the sample.  $^{1}$ H NMR (400 MHz, DMSO- $^{1}$ 6)  $\delta$  (ppm) 4.86–4.76 (m, 2H), 4.68 (dd, J = 18.6, 7.6 Hz, 1H), 4.11–3.92 (m, 4H), 3.73 (s, 2H), 3.38 (s, 1H), 2.29 (s, 4H), 1.52 (s, 4H).

#### 2.2.2.2 Synthesis of poly(D-sorbitol adipate)

Poly(D-sorbitol adipate) (PDSA) was synthesized using the analogous procedure as described for poly(xylitol adipate) but the crude product was dialyzed to remove oligomers using water as dialysis medium and a membrane with a cut-off molar mass of 1000 g·mol<sup>-1</sup>. <sup>1</sup>H NMR spectroscopy was used to confirm the purity of the samples. <sup>1</sup>H

NMR (400 MHz, DMSO- $d_6$ )  $\delta$  (ppm) 4.97–4.61 (m, 2H), 4.55–4.30 (m, 2H), 4.28–3.82 (m, 3H), 3.70 (d, J = 49.1 Hz, 2H), 3.58–3.33 (m, 2H), 2.37–2.17 (m, 4H), 1.64–1.42 (m, 4H).

# 2.2.2.3 Synthesis of stearoyl grafted poly(xylitol adipate) and poly(D-sorbitol adipate)

Poly(xylitol adipate) and poly(D-sorbitol adipate) with a number average molar mass  $M_n$  of 5,000 g·mol<sup>-1</sup> and 3,500 g·mol<sup>-1</sup>, respectively, were used for further modification with stearoyl chains using a standard procedure. PXA or PDSA dissolved in DMF/THF (50/50 v/v) were charged into a three neck (100 mL) round bottom flask, equipped with condenser and magnetic stirrer. Triethylamine was added as an acid scavenger. Stearoyl chloride was dissolved in THF at room temperature and added dropwise to the reaction mixture. The temperature was raised to 80 °C, and the reaction was stopped after 6 h. The solvent was removed in a rotary evaporator. To remove the salt of trimethylamine and unreacted trimethylamine, the crude product was dissolved in DCM and extracted four times with brine. The organic phase was collected and dried with magnesium sulfate. The crude product was precipitated in *n*-hexane for products with less than 40 mol% grafted chains and in methanol for products with more than 40 mol% grafting, to remove unreacted fatty acid. A slightly brownish solid product was obtained. PXA-g-S: <sup>1</sup>H NMR (500 MHz, CDCl<sub>3</sub>)  $\delta$  (ppm): 5.47–4.99 (m, 3H), 4.54–3.7 (m, 4H), 2.35 (d, J = 42.4 Hz, 10H), 1.67 (s, 10H), 1.26 (s, 84H), 0.89 (t, J = 6.9 Hz, 9H). PDSA-g-S: <sup>1</sup>H NMR (400 MHz, CDCl<sub>3</sub>) δ (ppm): 5.65–4.76 (m, 4H), 3.5–4.5 (m, 4H), 2.35 (m, 12H), 1.64 (s, 12H), 1.43-1.15 (m, 112H), 0.87 (t, J = 6.8 Hz, 12H).

#### 2.2.3 Preparation of nanoparticles

Nanoparticles were prepared using the interfacial deposition method described elsewhere  $^{83}$  with slight modification. In this approach, 150  $\mu L$  of 15 mg·mL $^{-1}$  polymer solution in THF was added slowly to 1.7 mL hot water (above the melting temperature of the polymer) with constant vortexing for 5 min at 45,000 rpm. Turbid dispersions were obtained which were further homogenized using silentCrusher S (Heidolph Instruments GmbH, Schwabach, Germany) for 3 min. 300  $\mu L$  cold water was then added for immediate solidification of the particles with vortexing. The organic solvent and small amounts of water were evaporated in a rotary evaporator. A small amount of water was again added to make a 0.1% w/v dispersion.

#### 2.2.4 Instrumentation

#### 2.2.4.1 NMR spectroscopy

 $^{1}$ H NMR spectra of grafted and non-grafted polyester backbones were recorded with a Varian Gemini 400 spectrometer at 400 MHz and 27 °C. Approximately 30 mg of polymer were dissolved in 0.8 mL of CDCl<sub>3</sub> or DMSO- $d_6$  as solvents, purchased from Armar Chemicals (Döttingen, Switzerland). The NMR spectra were interpreted using MestRec v.4.9.9.6 (Mestrelab Research, Santiago de Compostela, Spain). The assignment of the peaks was made using Chem Office 2004-ChemDraw ULTRA 8, software from Cambridge, UK.

#### 2.2.4.2 Size exclusion chromatography (SEC)

SEC measurements were performed on a Viscotek GPCmax VE 2002 using HHRH Guard-17360 and GMHHR-N-18055 columns and a refractive index detector was used (VE 3580 RI detector, Viscotek, GmbH, Waghäusen, Germany). THF was used as eluent. For all samples, the concentration was 3 mg·mL<sup>-1</sup> and the flow rate was 0.1 mL·min<sup>-1</sup>. For PXA and PDSA, the measurements were done with DMF containing 0.01 M LiBr as mobile phase in a thermostated column oven kept at 80 °C. The calibration standards for measurements in THF and DMF were polystyrene and poly(methyl methacrylate), respectively.

#### 2.2.4.3 Differential scanning calorimetry (DSC)

Thermal properties of the polymers were measured using a differential scanning calorimeter (DSC, Mettler Toledo DSC823e module, Mettler-Toledo GmbH, Greifensee Switzerland). All samples were scanned within the temperature range of –50 to 80 °C with a heating rate of 10 °C·min<sup>-1</sup>. 8 mg to 12 mg of sample material was enclosed in an aluminum pan and placed in the DSC sampler at room temperature. All measurements were performed under constant flow of nitrogen (10 mL·min<sup>-1</sup>).

#### 2.2.4.4 Dynamic light scattering (DLS)

All samples were measured in Plastibrand PMMA disposable cuvettes (Brand GmbH, Wertheim, Germany) with the ALV-NIBS/HPPS spectrometer (ALV-Laser Vertriebsgesellschaft M.B.H., Langen, Germany). As a light source, a He–Ne laser with a power of 3 mW and a wavelength of  $\lambda$  = 632.8 nm was used. The scattering intensity was

recorded by a photomultiplier at an angle of 173°, and the temporal intensity fluctuations were recorded with a Multiple Tau digital correlator ALV transfer 5000/E (Vertriebsgesellschaft M.B.H., Langen, Germany). The analysis was performed with the ALV Correlator Software 3.0 through the "regularized fit" mode.

#### 2.2.4.5 Negative-staining TEM

Samples for negative-staining TEM were prepared by spreading 3  $\mu$ L of the dispersion onto a Cu grid coated with a Formvar® film (Plano, Wetzlar, Germany). The excess liquid was blotted off after 30 s. Afterward, the grid was placed on a droplet of 1 wt% aqueous uranyl acetate solution and drained off after 1 min. The dried specimens were observed with a Zeiss EM 900 transmission electron microscope (Carl Zeiss Microscopy GmbH, Oberkochen, Germany). Micrographs were taken with a SSCCD SM-1K-120 camera (TRS, Moorenweis, Germany).

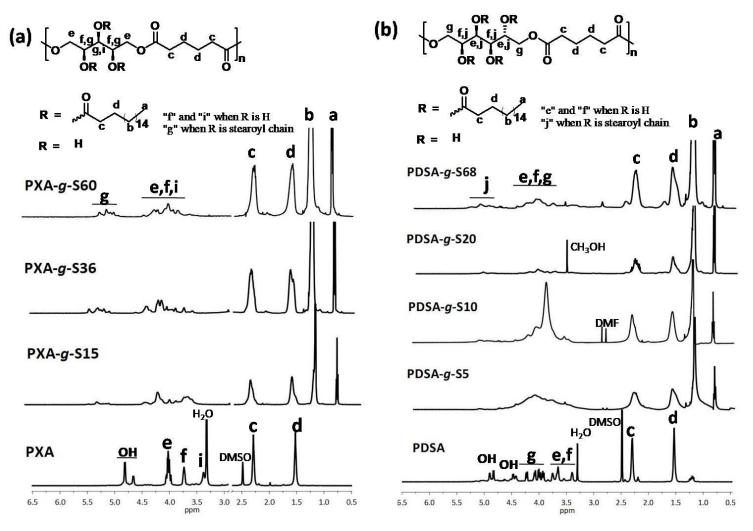
#### 2.2.4.6 X-ray diffraction (XRD)

X-ray diffraction patterns were recorded with a 2D detector (Vantec 500, Bruker, AXS, Madison, WI, USA) using Ni-filtered and pinhole collimated Cu K $\alpha$  radiation. The exposure time was 15 min and the sample to detector distance was 9.85 and 27.7 cm for wide and small angle scattering experiments, respectively. The samples were held in glass capillaries ( $\emptyset$  1 mm, Hilgenberg, GmbH, Malsfeld, Germany).

#### 2.3 RESULTS AND DISCUSSION

#### 2.3.1 Polymerization and grafting

The enzymatic syntheses of PXA and PDSA are carried out by a polycondensation (basically a polytransesterification) reaction of xylitol and D-sorbitol, respectively, with divinyl adipate. Since the enzyme reacts preferably with primary hydroxyl groups at reasonably low temperatures, the secondary hydroxyl groups remain unreacted.<sup>66</sup> As a result, linear PXA and PDSA samples with pendant OH-groups are obtained. PDSA is a water-soluble polymer whereas PXA forms a fine suspension in water. Dynamic light scattering of a 10 g·L<sup>-1</sup> suspension of PXA is given in Figure A1 (Appendix).



**Figure 2.1.** <sup>1</sup>H NMR spectra of (a) grafted and non-grafted poly(xylitol adipate), and (b) grafted and non-grafted poly(D-sorbitol adipate) recorded at 27 °C using CDCl<sub>3</sub> and DMSO-d<sub>6</sub> as a solvent for grafted and non-grafted polymers, respectively.

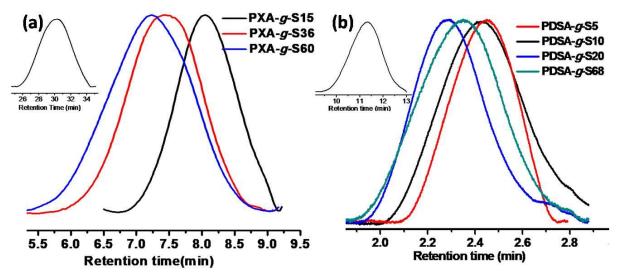
In the second step of the synthesis, the functional polyesters are grafted with stearoyl chains resulting in different degrees of grafting.  $^{1}$ H NMR spectra of grafted and non-grafted PXA and PDSA are shown in Figure 2.1. The relative increase in the intensity of the peaks belonging to the stearoyl side chains indicates the degree of grafting. The quantitative determination of the degree of grafting is calculated by taking into account the integral values of peaks a and c using Equation 2.1 for PXA-g-Sx and Equation 2.2 for PDSA-g-Sx.

mol% degree of grafting = 
$$\frac{0.44 \times a}{c - 0.67a} \times 100$$
 2.1

mol% degree of grafting = 
$$\frac{0.33 \times a}{c - 0.67a} \times 100$$
 2.2

In equations 2.1 and 2.2 a stands for the integration area of methyl group protons of stearoyl chains while c stands for the integration area of protons of methylne next to the carbonyl group of the polymer backbone and stearoyl side chains. Using Equations 2.1 and 2.2, the mol% of grafted OH groups of polymer backbone calculated for PXA was 15, 36, and 60, whereas, for PDSA, the respective values are 5, 10, 20, and 68.

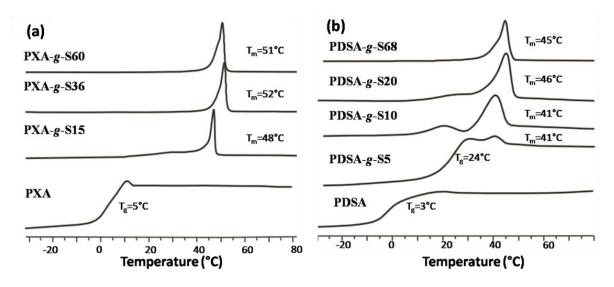
The grafting is further verified by size exclusion chromatography (see Figure 2.2), where a shift of the peak maximum to lower retention times with increasing degrees of grafting occurs.



**Figure 2.2.** Size exclusion chromatography (SEC) traces of (a) stearoyl grafted poly(xylitol adipate) in THF and (b) SEC traces of stearoyl grafted poly(D-sorbitol adipate) in THF. The insets show the SEC traces of the polymer backbones PXA and PDSA, respectively, in DMF.

Due to the insolubility of polymer backbones PXA and PDSA in THF, the measurements are carried out in DMF as eluent while for all other grafted polymers THF is employed. The number average molar masses and the polydispersity index *PDI* defined as  $M_W/M_R$  together with thermal properties of all polymers are given in Table 2.1.

Thermal properties of grafted and non-grafted PXA and PDSA, respectively, are determined by differential scanning calorimetry. PXA and PDSA are amorphous polymers with a glass transition temperature  $T_g$  of 5 and 3 °C, respectively. However, all graft copolymers are semicrystalline indicated by the melting endotherms. All details on the phase transitions are summarized in Table 2.1.



**Figure. 2.3.** DSC traces of (a) grafted and non-grafted PXA and (b) grafted and non-grafted PDSA. The measurements are carried out with a heating rate of 10 °C·min<sup>-1</sup>.

The melting temperature  $T_m$  is determined from the maximum of the endothermal peak during the heating scan. DSC traces of graft copolymers and polymer backbones are shown in Figure 2.3. As already mentioned, the grafting of saturated fatty acids to this type of polyesters induces crystallinity caused by side-chain crystallization. The melting temperature is about 50 °C in case of PXA-g-Sx, whereas for PDSA-g-Sx, the melting peak occurs between 41 and 45 °C. For very low degrees of grafting, both a glass transition temperature and a melting endotherm can be observed in the DSC traces.

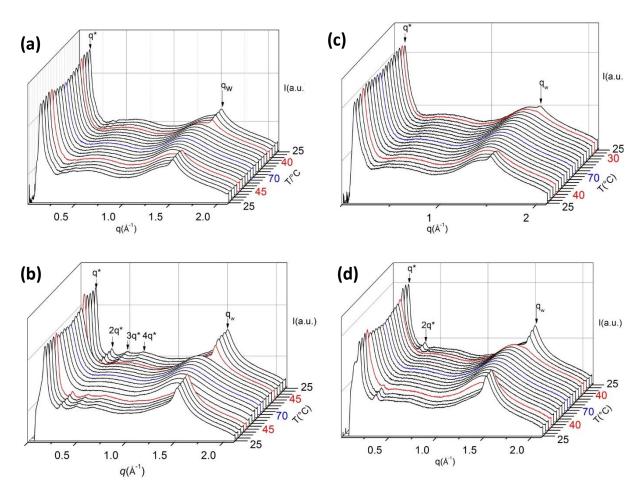
**Table 2.1** The volume fraction of grafted chains,  $\phi_{stearoyb}$   $M_n$ , PDI,  $T_m$ ,  $T_g$  and  $\Delta H_m$  of grafted and non grafted polymers.

Polymer	$oldsymbol{\Phi}_{Stearoyl}$ 5	<i>M</i> <sub>n</sub> (g·mol <sup>-1</sup> )	PDI	<i>T<sub>m</sub></i> (°C)⁴	<i>T<sub>g</sub></i> (°C)⁴	$\Delta H_m$ (J·g <sup>-</sup> 1) <sup>4</sup>
PXA	-	5,0001	2.41	-	5	
PXA- <i>g</i> -S15	0.37	7,3002	$2.3^{3}$	48	20	60
PXA- <i>g</i> -S36	0.58	10,6002	$2.6^{3}$	52	-	100
PXA- <i>g</i> -S60	0.69	14,6002	$1.8^{3}$	51	-	85
PDSA	-	$3,500^{1}$	$1.9^{1}$	-	3	-
PDSA-g-S5	0.15	4,3002	1.43	41	24	1.15
PDSA-g-S10	0.30	4,8002	1.93	41	-	36
PDSA-g-S20	0.43	5,8002	$1.5^{3}$	46	-	136
PDSA-g-S68	0.71	12,2002	$1.7^{3}$	45	-	73

<sup>1</sup>Obtained from GPC using DMF as eluent. <sup>2</sup>Calculated on the basis of % degree of grafting from the <sup>1</sup>H NMR spectra. <sup>3</sup>Obtained from GPC using THF as eluent. <sup>4</sup>Obtained from DSC at a heating rate of 10 °C⋅min<sup>-1</sup>. <sup>5</sup>Volume fraction of stearoyl side chains estimated by Material Studio 4.1

Combined SAXS and WAXS investigations are carried out for polymers in bulk. These comb-like polymers show nanophase separation that arises from the immiscibility of the side chains with the polymer backbone. Ordering of these nanophases strongly depends on the lipophilic volume fraction of the side chains. For polymers having a relatively low degree of grafting, a low volume fraction of the side chains is obtained, for instance, PXA-*g*-S15 (Figure 2.4(a)) has a volume fraction of the side chains of 0.37.

For this sample, a peak in the small angle regime at  $q^* = 0.1136 \text{ Å}^{-1}$  (the corresponding d-spacing is 55.3 Å) during the heating scan is observed. In the wide angle region, only one single peak is visible ( $q_w = 1.5222 \text{ Å}^{-1}$ ) superimposed by diffuse scattering. Assuming a hexagonal ordering of the side chains, this peak corresponds to the (110) direction of the hexagonal lattice, having a lattice parameter a = 4.77 Å. This can also be assigned as pseudo hexagonal rotator phase  $R_H$  which is typically appears for alkyl grafted comb like polymers.<sup>88,201</sup> At the melting temperature of 48°C, the peak in the wide angle region disappears whereas an amorphous halo remains at lower q-values and the peak in the small angle region becomes broader.



**Figure. 2.4.** Combined SAXS and WAXS traces during heating and cooling cycles (5 °C step from 25°C to 70 °C and back to 25 °C) of (a) PXA-*g*-S15 (b) PXA-*g*-S36 (c) PDSA-*g*-S10 and (d) PDSA-*g*-S68.

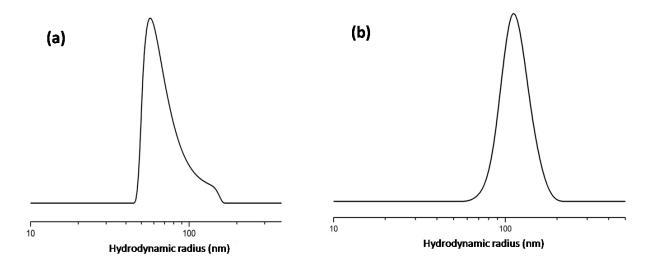
For polymers with relatively high degrees of grafting, a more ordered nanophase separation is observed, e.g. in PXA-g-S36 (the volume fraction of hydrophobic side chain is 0.58). Combined SAXS and WAXS heating and cooling scans of PXA-g-S36 are shown in Figure 2.4(b). At low temperature, one prominent peak in the small angle region  $q^*$  and several higher order peaks as integral multiples of  $q^*$  are visible, indicating a lamellar structure caused by nanophase separation of the polymer backbone and the side chains (d = 38.1 Å) followed by crystallization of side chains.<sup>88</sup> In the wide angle region, only one single peak appears  $q_w$ . The lattice parameter a = 4.78 Å is nearly identical with that of PXA-g-S15. At the melting temperature of 52°C, the first order peak in the small angle region becomes broader and the higher order peaks disappear. This behavior indicates that the lamellar structure is significantly stabilized by the side chain crystallization. After cooling below the crystallization temperature of 45 °C, the higher order peaks appear again.

The sample PDSA-g-S10 (Figure 2.4(c)) with a volume fraction of 0.30 of side chains shows a similar scattering pattern as PXA-g-S15 with a slightly larger d-spacing of 57.1 Å. The sample PDSA-g-S68 (Figure 2.4(d)) with higher side chain content (volume fraction of 0.71) shows in the small angle regime again the typical scattering pattern of a lamellar phase with a d-spacing of 35.5 Å. The complete data of all SAXS and WAXS measurements are given in Tables A1–A8 in the Appendix. It is interesting to note that the lattice parameters of the hexagonal rotator phase remain the same, independent of the degree of grafting.

#### 2.3.2 Nanoparticles

#### 2.3.2.1 Dynamic light scattering

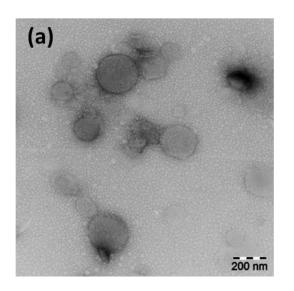
Dynamic light scattering is employed to determine the size of nanoparticles formed by the graft copolymers. Nanoparticles were prepared by the interfacial deposition method (also called nanoprecipitation method).83 The polymer dispersion in water at a concentration of 1 g·L<sup>-1</sup> at 25 °C is used. The average hydrodynamic radius of PXA-g-S15 is found to be 69 nm whereas for PDSA-g-S10 it is 105 nm. The reason behind the difference in particle sizes of both samples could be the overall hydrophilicity of the polymer chains. Since PDSA-g-S10 is more hydrophilic than PXA-g-S15, it shows a comparatively higher hydrodynamic radius in water. The particle size distributions of the respective polymer dispersions are shown in Figure 2.5. Since the size and shape of the nanoparticles are important factors for *in vivo* drug release,<sup>27,202,203</sup> the control of these parameters is important. The size of the nanoparticles can be tailored by choosing appropriate solvents and temperatures for the interfacial deposition method. Any solvent that is miscible with water and that can dissolve the polymer as well will be appropriate for this method.<sup>204</sup> A solvent with poor water miscibility results in a decrease in interfacial tension towards the oil in water interface during the preparation process and results in an increase in particle size.205

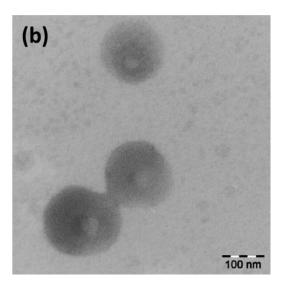


**Figure 2.5.** (a) Hydrodynamic radius distribution of PXA-g-S15 nanoparticles in water with a concentration of 1 g·L<sup>-1</sup> at 25°C and (b) hydrodynamic radius distribution of PDSA-g-S10 nanoparticles (1 g·L<sup>-1</sup> in water at 25°C).

#### 2.3.2.2 Negative-staining transmission electron microscopy

To study the morphology of the nanoparticles, negative-staining TEM on dried nanoparticles was carried out using uranyl acetate as the staining agent. The negative stained TEM images are shown in Figure 2.6.





**Figure 2.6.** Negative-staining electron micrographs of (a) 0.1 wt% dispersion of PXA-*g*-S15 and (b) 0.1 wt% dispersion of PDSA-*g*-S10.

It shows spherical morphologies of the nanoparticles which is a typical behavior of particles formed upon surface energy minimization. It can be seen that PXA-g-S15 forms homogeneous nanoparticles (see Figure 2.6(a)) whereas for PDSA-g-S10 some kind of

additional aggregation in the nanoparticles is observed (see Figure 2.6(b)). Since the geometry, surface properties and internal structure of nanoparticles strongly influence the drug incorporation,<sup>203</sup> studies are in progress to investigate these characteristics in our graft copolymer systems in more detail.

#### 2.4 CONCLUSIONS

In conclusion, a simple approach for synthesizing sugar based functional polyesters has been used to produce hydrophilic polymers, which were grafted with stearoyl chains to obtain amphiphilic graft copolymers. Unlike the initial amorphous polyester backbone, the grafted polyesters are semi-crystalline in nature. These amphiphilic comb-like polymers show a nanophase separation leading to lamellar morphologies which are more pronounced in the case of a relatively high degree of grafting, such as for PXA-g-S36 and PDSA-g-S68. However, for a small degree of grafting this nanophase separation is less ordered, which results in only one peak in the SAXS traces. A diffraction peak at higher scattering angles (WAXS) in all grafted copolymer samples corresponds to the (110) reflection which indicates the pseudo hexagonal rotator phase that exists until the melt temperature of the polymers is reached. Furthermore, these polymers are able to form well-arranged nanoparticles, prepared by the interfacial deposition method. It would be interesting, in the future, to explore the morphology and properties as e.g. the hydrolytic stability of the nanoparticles formed from these polymers and to develop their applications in drug delivery systems. Due to the biodegradability of these nanoparticles, they might be an alternative to many Pluronic® based systems.

#### **CHAPTER 3**

# 3 POLY(GLYCEROL ADIPATE)-G-OLEATE AND THE GMO/WATER SYSTEM

#### 3.1 INTRODUCTION

Lipase-catalyzed polyester synthesis was a promising approach for synthesis of biocompatible polymers during the last two decades as it is a green process, 3,13,65,206-208 and it also offers a simple way to synthesize functional polyesters. 13,35,54,65,85,208-212 Poly(glycerol adipate) (PGA) is a hydrophilic, biocompatible, and biodegradable polyester with many potential biomedical and pharmaceutical applications.<sup>83</sup> The most important advantage of PGA, as compared to other biodegradable polyesters, such as polylactide and poly(ε-caprolactone), is the pendant hydroxyl functionality at each structural repeat unit that imparts a hydrophilic character to the polymer and offers an opportunity for convenient post-polymerization reactions. Thus, we and several others synthesized comb-like amphiphilic copolymers based on the PGA backbone, 27,29,83,90,91,213 including amphiphilic graft copolymers of PGA and fatty acids of various chain lengths, obtained via a simple condensation reaction between pendant hydroxyl groups and fatty acid chlorides. The resulting amphiphilic graft polymers are able to self-assemble in water into self-stabilizing well-defined nanoparticles of diverse shapes with enhanced drug loading efficiency.83,214 The length of acyl chains and the degree of substitution play an important role for the structure formation in bulk and in nanoparticles.<sup>27</sup> For example, depending upon the degree of substitution, PGA with stearate side chains is found to form spherical nanoparticles with well-defined phase-separated lamellar internal structure at higher degrees of substitution and polygonal nanoparticles with pseudo-hexagonal internal structure at lower degree of acylation.88 Long and saturated all-trans acyl-side chains of PGA-g-acyl polymers organize into a crystal structure in bulk and nanoparticles which could have an adverse effect on the loading and release properties of these nanoparticles in pharmaceutical and biomedical applications.<sup>215</sup> Therefore, the design of amphiphilic graft polymers of non-crystallizable long side chains would be more attractive for practical applications. The oleate chain is a C18 chain with a cis double bond between C9 and C10 that hinders crystallization strongly. The oleate residue would be an ideal option

for achieving a completely amorphous amphiphilic PGA based graft copolymer, with potential applications not only in drug delivery systems but also, due to the identical chain structure of the oleate side chains and the hydrophobic oleate tail of glycerol monooleate (GMO) (Scheme 3.1) in tuning the properties of the liquid crystalline phases of GMO and GMO/water, possibly by the integration of the oleate side chains into the lipid bilayers. $^{216}$ - $^{218}$ 

Due to the partial oil solubility, GMO is commonly used as a food emulsifier.  $^{104}$  It self-assembles into a variety of liquid crystalline structures in the presence of different amounts of water and as a function of temperature,  $^{121,149,155,219}$  including the important inverse bicontinuous cubic phases with water channels separated by lipid bilayers.  $^{220}$  The diameter of the water channel in these structures predominantly controls the extent of drug or protein loading and the release behavior.  $^{221,222}$  Furthermore, large molecules as protiens could be accommodated only in highly swollen and enlarged water channels of the cubic phases. Therefore, tuning the swelling and enlargement of the water channels is extremely important for enhanced applications of the cubic phases as biocompatible host in numerous applications, such as biosensors and higher loading efficiency for biologically and pharmaceutically active ingredients.  $^{168,221-223}$  To achieve this, the introduction of a third component, mostly a low molar mass additive, such as nonionic octyl- $\beta$ -D-glucopyranoside ( $\beta$ -Glc-OC8),  $^{221}$  the charged surfactant-doped system dioctyl sodium sulfosuccinate,  $^{221}$  neutral sucrose stearate,  $^{223}$  charged lipids,  $^{222}$  cholesterol,  $^{222}$  and nucleic acids,  $^{224}$  to name a few, to the GMO/water system has been explored.

For certain applications, such as nasal and intravenous drug delivery, <sup>225</sup> the bulk liquid crystalline phases could be fragmented and stabilized in aqueous dispersions into submicron size particles with cubic geometry maintaining the well-defined internal cubic structure, generally named as cubosomes. The commercially available Pluronic® F127, an amphiphilic triblock copolymer of poly(ethylene glycol) and poly(propylene oxide), has been found to offer the most effective and long-term steric stability to the cubosomes. <sup>131,225–229</sup> However, several other amphiphilic species, including PEG-lipid copolymers, <sup>114,230</sup> polyethoxylated stearates (Myrj series), <sup>231</sup> modified cellulose, <sup>232</sup> and polysorbate 80<sup>231</sup> have also been investigated.

The main objective of the current study is to employ amphiphilic oleate grafted PGA, PGA-*g*-oleate for systematic investigation of its influence on the GMO/water mesophase behavior and its potential application as a nanoparticle stabilizer in aqueous dispersions.

Thus, the enzyme-catalyzed synthesis of linear PGA was carried out using divinyl adipate and glycerol, which was subsequently transformed into PGA-g-oleate (PGA-g-Ox) by reacting with oleoyl chloride. Samples with various degrees of grafting were synthesized and characterized by differential scanning calorimetry (DSC), and small angle X-ray scattering (SAXS) for nanophase separation. The samples are named PGA-g-Ox, where x represents the degree of grafting (mol% of the pendant OH groups esterified). Systematic studies were carried out at room temperature on the GMO/PGA-g-O22/water ternary systems and a ternary phase diagram was constructed. It was observed that the addition of polymer to the GMO/water system induces swelling of the cubic phase and enlargement of water channels. Preliminary investigations on the potential application of PGA-g-O22 as a steric stabilizer of structured nanoparticles in aqueous dispersions were carried out using different transmission electron microscopy (TEM) techniques.

**Scheme 3.1**: (a) Enzymatic synthesis of poly(glycerol adipate) (PGA) and post-polymerization modification with oleoyl chloride and (b) synthesis of glycerol monooleate (GMO).

#### 3.2 EXPERIMENTAL SECTION

#### 3.2.1 Materials

Glycerol ( $\geq$ 99.5%), anhydrous tetrahydrofuran (THF, water content 0.02%), oleoyl chloride ( $\geq$  89%), and Novozym 435 (derived from *Candida antarctica* type B (CAL-B) immobilized on an acrylic macroporous resin) (5000 U·g<sup>-1</sup>, water content 1-2%) were purchased from Sigma Aldrich. Novozym 435 was dried under vacuum at 4 °C and over  $P_2O_5$  for 24 h before use. Divinyladipate (DVA, 96%) was purchased from TCI-Europe and was used as received. Acetone, *n*-hexane, ethyl acetate, methanol, dichloromethane (DCM), and pyridine were purchased from Carl Roth. Solketal (97%) was purchased from Alfa Aesar and used as received.

#### 3.2.2 Syntheses

#### 3.2.2.1 Synthesis of poly(glycerol adipate) (PGA)

The PGA backbone was synthesized by enzymatic solution polymerization according to the procedure described previously. 27,233 Briefly, glycerol (22.6 g, 245 mmol) and an equimolar amount of divinyl adipate (50.7 g, 245 mmol) were charged into a 250 ml three neck round bottom flask equipped with an overhead mechanical stirrer and a reflux condenser containing CaCl<sub>2</sub> drying tube at its outlet. Subsequently, 45 ml of THF was added to the reaction flask. The mixture was stirred for 30 min at 50 °C, and then CAL-B (1.42 g Novozym 435, 2 wt% with respect to the monomers) was added to start the polymerization. The reaction mixture was cloudy at the start due to the insolubility of glycerol in THF. However, as the reaction proceeded the turbidity disappeared upon the formation of oligomers. After 11 h the reaction mixture was diluted by the addition of a small amount of THF and the enzyme beads were filtered off. THF was removed by rotary evaporator to recover the final product (49 g) as a slightly yellow and viscous polymer that was used without further purification. The molar mass of PGA was measured using GPC as  $M_n = 4,800$  g·mol<sup>-1</sup>, with a polydispersity index (PDI) of 2.0. The <sup>1</sup>H NMR and inverse-gated <sup>13</sup>C NMR spectra are shown in Figure A2 in the Appendix and Figure 3.2(a), respectively. The assignment of the peaks was made following the literature. 57,197,234

#### 3.2.2.2 Syntheses of poly(glycerol adipate)-g-oleate (PGA-g-Ox)

The acylation of the PGA backbone was achieved with various degrees of grafting by the reaction between pendant hydroxyl groups of the PGA backbone and oleoyl chloride in analogy to the grafting procedure with different fatty acids.<sup>27,83,233</sup> A typical procedure for 15 mol% intended degree of grafting was in such a way that PGA (4.0 g, 19.8 mmol) was dissolved in 50 ml THF in a 100 ml three neck round bottom flask equipped with a condenser and magnetic stirrer. After the addition of pyridine (3.9 g, 49 mmol) the reaction flask was transferred to an ice bath. After cooling it for approximately 30 min, the oleoyl chloride (0.88 g, 2.97mmol) diluted with 5 ml THF was added drop-wise at 0°C. The reaction was allowed to proceed at room temperature for approximately 20 min and then under reflux for 3 h. The reaction mixture was filtered to remove the pyridinium salt. The solvent was evaporated by rotary evaporator, and the crude product was dissolved in dichloromethane (DCM) and extracted three times with brine. The organic phase was separated and dried over sodium sulfate. To ensure the complete removal of the unreacted fatty acid, the filtrate was concentrated by rotary evaporator and precipitated three times in ice-cold *n*-hexane. The purification of graft polymers with a degree of grafting greater than 40 mol% was carried out via column chromatography using the eluent (1) acetone : n-hexane = 5 : 95 v/v and (2) acetone. The characteristic <sup>1</sup>H NMR and inverse-gated <sup>13</sup>C NMR spectra are shown in Figure A3 and Figure A4(b), respectively, in the Appendix. The assignment of the peaks was done according to the literature. 57,58,234

#### 3.2.2.3 Synthesis of glycerol monooleate (GMO)

Glycerol monooleate was synthesized from solketal, and oleoyl chloride following the procedure reported elsewhere.<sup>235</sup> Briefly, solketal (5 g, 37.8 mmol), anhydrous THF (80 ml), and pyridine (6 ml) were added into a 100 ml three neck round bottom flask, equipped with a septum, and magnetic stirrer bar. The reaction flask was placed in an ice bath. Oleoyl chloride (13.6 g, 45.3 mmol) was added drop-wise to the reaction mixture. The reaction was allowed to run for 3 h at room temperature. The pyridinium salt was removed by filtration and the solvent was removed by rotary evaporator. The crude product was dissolved in DCM and extracted three times with water. In the next step, cleaving of the solketal was carried out in 2.0 N HCl in methanol for 5 h. The acid was neutralized with 1.0 N NaOH. The reaction mixture was concentrated in a rotary evaporator, and the crude product was dissolved in DCM and washed three times with

brine. The organic phase was concentrated by evaporating most of the solvent, and the final product was recovered after column chromatography using (1) n-hexane : ethyl acetate 70/30 v/v and (2) n-hexane : ethyl acetate 50/50 v/v as the eluent. The purified GMO was a mixture of G1MO (glycerol-1-monooleate) 92 mol% and G2MO (glycerol-2-monooleate) 8 mol% (Scheme 3.1) due to acyl migration in acidic media during the cleaving step. $^{236}$  The purity of the product was confirmed by  $^{1}$ H NMR spectroscopy as shown in Figure A5 in the Appendix.

#### 3.2.3 Polymer characterization

 $^{1}$ H NMR spectra and inverse gated (quantitative  $^{13}$ C NMR) spectra were recorded on a Varian Gemini NMR spectrometer at 400 MHz and 126 MHz respectively at 27 °C in CDCl<sub>3</sub>. For  $^{1}$ H NMR spectroscopy the concentration of polymer was  $\sim$ 4 % w/v in CDCl<sub>3</sub>. For  $^{13}$ C NMR spectroscopy the concentration of polymer was  $\sim$ 30 % w/v in CDCl<sub>3</sub>.

The number average molar mass  $(M_n)$ , the weight average molar mass  $(M_w)$ , and the polydispersity index  $(M_w/M_n)$  were measured using Viscotek GPC<sub>max</sub> VE 2001 with a column set CLM3008 (guard column) and 1GMHHR (analytical column) equipped with VE 3580RI refractive index detector using polystyrene standards and THF as the eluent with a flow rate of 1 ml·min<sup>-1</sup> at 22°C (column temperature). The thermal behavior of the polymers was investigated by NETZSCH DSC 204F1 Phoenix. The samples were heated at 10 °C·min<sup>-1</sup> to 110°C, held for 10 min, followed by cooling to -80°C with 10 °C·min<sup>-1</sup>, held at -80°C for 10 min and then heated in the second heating run with 10 °C·min<sup>-1</sup> to 60°C. The glass transition temperature  $T_g$  was defined as the inflection point of the second heating run.

#### 3.2.4 Sample preparation for X-ray diffraction

Samples for X-ray diffraction studies were prepared by taking the desired amount of GMO and PGA-g-O22 in an Eppendorf tube and melt mixed at 50 °C with repeated cycles of spatulations and vortexing, followed by the addition of the desired amount of water and subsequent cycles of spatulations and vortexing for homogenous mixing. Each sample was stored at room temperature for 24 h before measurement. All compositions are given in wt%.

#### 3.2.5 Preparation of nanoparticles

PGA-g-O22 and GMO/PGA-g-O22 hybrid nanoparticles were prepared by the interfacial deposition method. <sup>27,83,233</sup> In detail, a solution of 10 mg of GMO/PGA-g-O22-90/10 v/v in 100  $\mu$ L acetone was added slowly to 1.5 ml water (40 °C) in an Eppendorf tube with constant vortexing for 2 min. The dispersion was further homogenized using a Heidolph SilentCrusher S for 5 min. The organic solvent and a small amount of water were removed by rotary evaporator at room temperature to have the final concentration of the dispersion of 1 % w/v.

#### 3.2.6 Dynamic light scattering

The particle size in aqueous dispersion was determined by an apparatus for and dynamic light scattering experiments simultaneous static Vertriebsgesellschaft mbH, Langen, Germany) with a He-Ne laser (632.8 nm, 20 mW). The thermostated sample cell was placed on a precision goniometer (±0.01°) that enabled the photomultiplier detector to move from 20° to 150° scattering angle. The intensity timecorrelation functions  $g^2(\tau)$  were recorded with an ALV-5000E multiple tau digital correlator. The minimal sampling time of this correlator was 12.5 ns. The cylindrical sample cells were made of Suprasil quartz glass by Hellman (Muellheim, Germany) and had a diameter of 10 mm. The pair correlation function f' was analyzed to obtain the effective diffusion coefficients  $D_{eff}$  of the dispersion. The hydrodynamic radius  $R_h$  of the equivalent hydrodynamic hard sphere was calculated via the Stokes-Einstein equation

$$R_h = \frac{k_B T}{6\pi \eta D_{eff}} \tag{3.1}$$

Where  $k_B$  is the Boltzmann constant and  $\eta$  is the viscosity of the solvent at temperature T.

#### 3.2.7 Negative stain transmission electron microscopy

The negatively stained samples were prepared by spreading 5  $\mu$ L of the nanoparticle dispersion onto a Cu grid coated with a Formvar-film (PLANO, Wetzlar, Germany). After 1 min excess liquid was blotted off with filter paper and 5  $\mu$ L of 1 wt% aqueous uranyl acetate solution was placed onto the grid and drained off after 1 min. The dried specimens were examined with an EM 900 transmission electron microscope (Carl Zeiss Microscopy GmbH, Oberkochen, Germany). Micrographs were taken with a SSCCD SM-1k-120 camera (TRS, Moorenweis, Germany).

#### 3.2.8 Cryogenic transmission electron microscopy

Vitrified specimens for cryo-TEM were prepared by a blotting procedure, performed in a chamber with controlled temperature and humidity using a LEICA grid plunger. A drop of the sample solution (1 mg·ml-1) was placed onto an EM grid coated with a holey carbon film (C-flat, Protochips Inc., Raleigh, NC). Excess solution was then removed with filter paper, leaving a thin film of the solution spanning the holes of the carbon film on the EM grid. Vitrification of the thin film was achieved by rapid plunging of the grid into liquid ethane held just above its freezing point. The vitrified specimen was kept below 108 K during storage, transfer to the microscope, and investigation. Specimens were examined with a LIBRA 120 PLUS instrument (Carl Zeiss Microscopy GmbH, Oberkochen, Germany), operating at 120 kV. The microscope is equipped with a Gatan 626 cryotransfer system. Images were taken with a BM-2k-120 Dual-Speed on axis SSCCD-camera (TRS, Moorenweis, Germany).

#### 3.2.9 X-ray diffraction

X-ray diffraction patterns were recorded with a 2D detector (Vantec 500, Bruker) using Ni-filtered and pin hole collimated Cu  $K_{\alpha}$  radiation. The exposure time was 15 min, and the sample to detector distance was 9.85 and 27.7 cm for wide and small angle scattering experiments, respectively. The samples were held in glass capillaries ( $\emptyset$  1 mm, Hilgenberg, Germany). For calculating the lattice parameters of the selected cubic phases, the X-ray diffraction patterns were recorded with an Anton-Paar compact Kratky camera using Ni-filtered and slit collimated Cu  $K_{\alpha}$  X-rays. The data were background corrected and desmeared.<sup>237</sup> The lattice parameter a of the cubic phase was calculated by  $^{104,238}$ 

$$d_{hkl} = \frac{2\pi}{q_{max}} = \frac{a}{\sqrt{h^2 + k^2 + l^2}}$$
 (3.2)

Where  $d_{hkl}$  is the distance between planes,  $q_{max}$  is the scattering vector at the peak maximum, and h, k, and l are the Miller indices of the scattering plane. The individual cubic phase is distinguished by the characteristic peak position ratios; for  $Pn3m = \sqrt{2}, \sqrt{3}, \sqrt{4}, \sqrt{6}, \sqrt{8}$  etc. (indexed as (hkl) = (110), (111), (200), (211), (220)) and for  $la3d = \sqrt{6}, \sqrt{8}, \sqrt{14}, \sqrt{16}, \sqrt{20}$  etc. (indexed as (hkl) = (211), (220), (321), (400), (420)). The lamellar phases show peak ratios of 1, 2, 3, 4 etc. Representative SAXS traces and their indices are given in Figure A7 in the Appendix.

#### 3.3 RESULTS AND DISCUSSION

# 3.3.1 Syntheses and grafting of poly(glycerol adipate) and glycerol monooleate

The enzyme-catalyzed synthesis of poly(glycerol adipate) (PGA) was carried out using glycerol and divinyl adipate in THF at 50°C in the presence of *Candida antarctica* Lipase B (CAL-B) (Scheme 3.1). Although PGA can also be produced by adipic acid or its alkyl esters instead of its vinyl esters, but to achieve high molar masses it is necessary to remove side products to shift the condensation equilibrium to the forward direction. The advantage of using divinyl adipate is that it is an irreversible procedure for lipase-catalyzed acylation, as the leaving group is vinyl alcohol that tautomerizes to acetaldehyde which is a gas, and it easily leaves the system resulting in high molar mass polymers, compared to polymers obtained from adipic acid or its alkyl ester, where the side product is water, methanol or ethanol<sup>197,209,239</sup> for which one must apply low pressure and high temperature. These conditions usually favour branching.<sup>65</sup> In this work, under the applied reaction condition, the regioselectivity of the enzyme was well under control as can be seen in <sup>13</sup>C NMR spectrum ( see Figure 3.2(a)).

From the spectrum the molar ratio of the various modes of the substituted glycerol unit was estimated from the integrated areas of the methine peak A-D: 1-substituted ( $T_G$ ): 1,2-disubstituted ( $L_{1,2}$ ): 1,3-disubstituted ( $L_{1,3}$ ): trisubstituted (D) = 4:4:90:2. On the basis of these data, the mol% regioselectivity at primary OH groups is calculated to 98 mol% using equation 3.3.57

% regional regional regional region of primary OH groups = 
$$\frac{T_G + (L_{1,2}) + 2(L_{1,3}) + 2(D)}{T_G + 2(L_{1,2}) + 2(L_{1,3}) + 3(D)} \times 100$$
 3.3

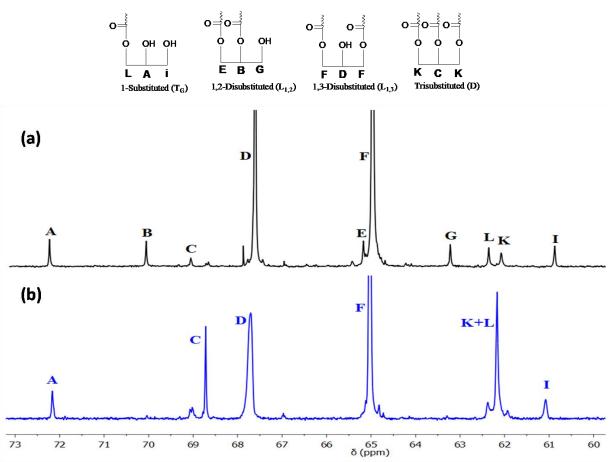
The mol% degree of branching of polymers are determined by Frechet equation (Equation 3.4)<sup>240</sup> or by Frey equation (Equation 3.5)<sup>241</sup>

mol% degree of branching = 
$$\frac{T_G + T_A + D}{T_G + T_A + L_{1,2} + L_{1,3} + D} \times 100$$
 3.4

% degree of branching = 
$$\frac{2D}{L_{1,2} + L_{1,3} + 2D} \times 100$$
 3.5

here,  $T_A$  is terminal adipic acid unit. Since the quantitative determination of  $T_A$  could not be done precisely. As a consequence the mol% degree of branching defined by Frey

(Equation 3.5) is preferred for our calculation. The mol% degree of branching is calculated to 4 mol%.

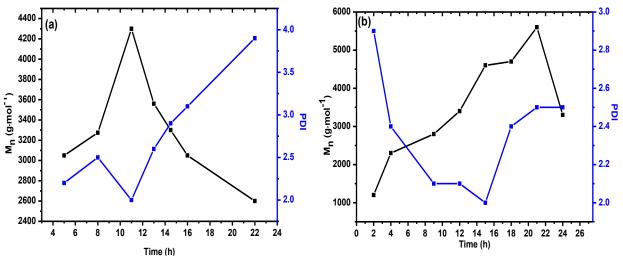


**Figure 3.2**. Expanded, inverse-gated <sup>13</sup>CNMR spectra of (a) PGA and (b) PGA-*g*-O22 recorded at 27°C in CDCl<sub>3</sub>.

Enzymatic transesterification is very sensitive to moisture, thus, certain moisture conditions can lead to depolymerization.<sup>208</sup> The source of moisture is the enzyme itself,<sup>61,70,242</sup> so careful optimization is needed to obtain the best results in terms of molar mass, the rate of reaction, and the polydispersity index. In the present work, the enzymatic polymerization was optimized at two different temperatures (30°C and 50°C). The corresponding change in molar mass and PDI with respect to time is shown in Figure 3.3.

In Figure 3.3a the reaction was carried out at 50°C using 2 wt% CAL-B with respect to the monomers in THF. This system gives the highest number average molar mass (4800 g·mol<sup>-1</sup>) and the polydispersity index of  $M_w/M_n = 2.0$  within 11 h. Beyond 11 h the molar

mass continuously decreases with increasing *PDI*. These findings indicate the presence of deacylation steps explained by Kobayashi.<sup>208</sup> The reason of this deacylation is the presence of trace amounts of water in the system.<sup>61,243</sup> The source of water is the enzyme itself, although the enzyme was dried over P<sub>2</sub>O<sub>5</sub> for 24 h and anhydrous THF was used for the reaction. The complete removal of water is not possible as there always remains a small amount of water within the active site of enzyme called "surface bound water".<sup>239</sup> This surface bound water is important for the enzyme activity as proteins are rigid in organic solvents.<sup>244</sup> It also increases the dielectric constant of the active site and makes it suitable to attack. A polar solvent such as THF, unbound the bounded water during the course of reaction that consequently leads to deacylation after some time.<sup>242</sup> However, reaction optimization studies at 30°C shown in Figure 3.3b reveal a slow reaction because of the low mobility of the oligomers as the highest molar mass was obtained after 25 h.



**Figure 3.3.** Optimizing the reaction conditions using 2 wt % CAL-B with respect to total mass of monomers at (a) 50°C (b) 30°C.

For the current work, PGA of molar mass of  $M_n = 4,800$  g·mol<sup>-1</sup> and the polydispersity index of  $M_w/M_n = 2.0$  obtained at 50 °C and 11 h of reaction time was considered for further grafting. It is worth mentioning here that no polymeric materials were formed in the absence of enzyme, indicating that the polymerization took place through enzyme catalysis, which is consistent with previous findings.<sup>57,245</sup>

In the next step of synthesis, the oleate side chains were grafted onto the PGA backbone by an esterification reaction between the pendant OH groups of the PGA and oleoyl chloride in THF at 80°C in the presence of pyridine.<sup>88</sup> The successful synthesis is

verified by <sup>1</sup>H NMR spectroscopy as shown in Figure 3.4, where, in addition to the signals of the PGA backbone, signals due to the oleate side chains are observed.

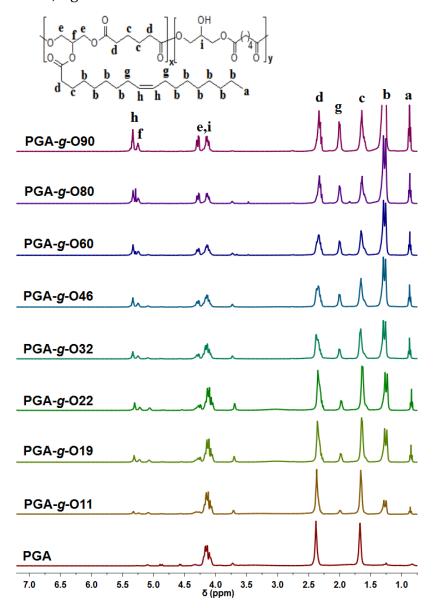


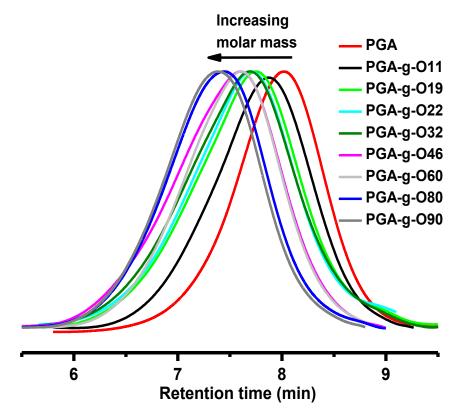
Figure 3.4: <sup>1</sup>H NMR spectra of PGA and the respective PGA-g-Ox, measured at 27 °C in CDCl<sub>3</sub>.

The degree of grafting is calculated from the respective <sup>1</sup>H NMR spectrum using the following formula

mol% degree of grafting = 
$$\frac{a \times 1.33}{d - 0.67a} \times 100$$
 (3.6)

where a represents the integral area of the methyl proton peak of oleate side chains and d is the combined area of the methylene protons of PGA backbone and the oleate side chain next to carbonyl groups.

In addition, the quantitative  $^{13}$ C NMR spectrum (see Figure 3.2(b)) helped to quantify the different types of the substituted glycerol unit as mentioned before. For PGA-g-022 the ratio of integrated areas of the methine peak A-D; 1-substituted : 1,2-disubstituted:trisubstituted = 7:0:70:23. On the basis of these data, the trisubstituted glycerol unit is calculated as 23% that fits with the degree of oleate grafting obtained using the  $^{1}$ H NMR spectrum.



**Figure 3.5:** GPC traces of the synthesized PGA and the respective PGA-*g*-Ox, measured in THF at 22 °C. The calibration was performed with polystyrene standards.

The polyester modification could also lead to the cleavage of the polymer backbone, but in this study, no significant cleavage was observed as a successive shift of the GPC traces (see Figure 3.5) to higher molar masses, with increasing degree of grafting is observed. Table 3.1 summarizes all data of the polymers under consideration.

Glycerol monooleate (GMO) was synthesized following the previously reported procedure.  $^{235}$  The final product was a mixture of G1MO (glycerol-1-monooleate, 92 mol%) and G2MO (glycerol-2-monooleate, 8 mol%) (calculated from the  $^{1}$ H NMR spectrum shown in Figure A4 in the Appendix).

**Table 3.1:** Characteristic data of the synthesized PGA and PGA-*g*-Ox.

Sample	M <sub>n</sub> (g/mol) <sup>a</sup>	$M_w/M_n^{\rm b}$	T <sub>g</sub> (°C) <sup>c</sup>	Φ <sub>oleate</sub> (vol.	d(Å)e
				%) <sup>d</sup>	
PGA	4,800	2.0	-24	0	-
PGA- <i>g</i> -011	5,600	2.1	-30	16	66.0
PGA- <i>g</i> -019	6,100	2.4	-33	24	51.5
PGA- <i>g</i> -022	6,400	2.0	-35	27	48.2
PGA- <i>g</i> -032	6,900	2.6	-38	33	44.9
PGA- <i>g</i> -046	7,700	2.6	-42	40	38.5
PGA- <i>g</i> -060	8,500	2.1	-47	46	35.3
PGA- <i>g</i> -080	9,800	2.3	-53	53	32
PGA- <i>g</i> -090	10,600	1.9	-57	56	30.9

<sup>&</sup>lt;sup>a</sup>All molar masses except for PGA are calculated on the basis of mol% degree of grafting calculated from the respective <sup>1</sup>H NMR spectra. Molar mass of PGA is obtained from GPC using THF as eluent against polystyrene standards (degree of polymerization is 24).

## 3.3.2 Characterization of PGA-g-Ox with nanodomains formed by oleate side chains

The flexibility and dynamics of the grafted chains control the crystallization of the side chains in graft copolymers with flexible backbone. PGA backbone was modified with all-trans stearate side chains that could crystallize and hence induced phase separation of the saturated alkyl side chains. PGA backbone was modified with all-trans stearate side chains that could crystallize and hence induced phase separation of the saturated alkyl side chains. PGGA in the system under investigation, however, the presence of cis-double bonds makes the oleate side chains incapable of packing into a crystalline structure. Therefore, completely amorphous graft copolymers were anticipated. Thus, the X-ray scattering profiles (Figure 3.6) of PGA and PGA-g-Ox exhibit only a typical broad amorphous halo in the wide angle regime ( $peak\ I$ ) with a maximum at approximately  $2\theta = 20^\circ$  and no Bragg reflections indicating the absense of crystals. The broad halo appears due to the average distance between neighbouring atoms in the amorphous state. In the small angle regime,  $peak\ II$  shifts to higher q-values with increasing grafting density which is an evidence of

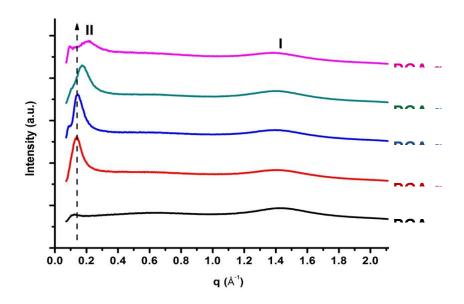
<sup>&</sup>lt;sup>b</sup>The polydispersity index  $M_w/M_n$  is obtained from the GPC data (Figure 3.5).

<sup>&</sup>lt;sup>c</sup>Obtained from the DSC thermograms shown in Figure 3.7.

<sup>&</sup>lt;sup>d</sup>Volume fraction of oleate side chain is calculated by Materials Studio software 4.1.

<sup>&</sup>lt;sup>e</sup>The characteristic length *d* was calculated from the respective *peak II* maximum in Figure 3.6.

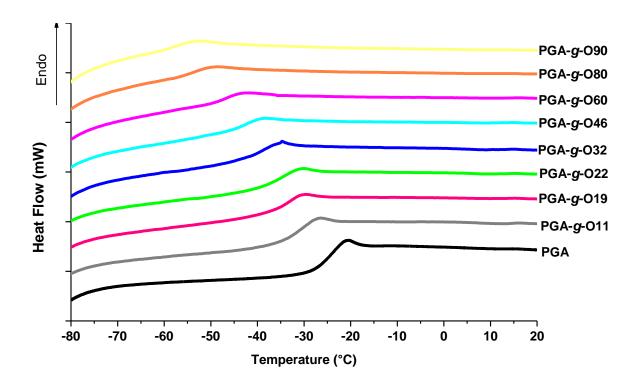
nanophase separation of the oleate side chains into nanodomains. According to Bragg's law, and the definition of the scattering vector q, peak II reflects a characteristic length of  $d = 2\pi/q_{max}$  in the range of 66 Å for PGA-g-O11 to 30.9 Å for PGA-g-O90. The decreasing length d with increasing degree of grafting can be attributed to the higher volume fraction of the nanodomains with increasing degree of grafting.



**Figure 3.6:** Combined SAXS and WAXS profiles of PGA and PGA-*g*-Ox. *Peak I* in the WAXS region of the trace indicates the amorphous halo and *peak II* in the SAXS region is caused by nanophase separation between the polymer backbone and grafted side chains.

The absence of higher order reflections, however, suggests the formation of less ordered structures and hence the bulk phase morphology could not be identified from SAXS data.<sup>83,91,233</sup> Further evidence of the amorphous nature of the synthesized graft polymers comes from differential scanning calorimetry (DSC) measurements (Figure 3.7) that exhibit only a glass transition temperature of the PGA backbone in unmodified PGA and all PGA-*g*-Ox samples.

A glass transition temperature of  $T_g \sim$  -24 °C is recorded for the unmodified PGA, which is consistent with the literature <sup>92</sup> and it decreases progressively for PGA-g-Ox from -32 °C to -60 °C when x is varied from 11 to 90. Thus, the grafted oleate side chains induce an internal plasticization by reducing the steric hindrance to the segmental mobility of the PGA.

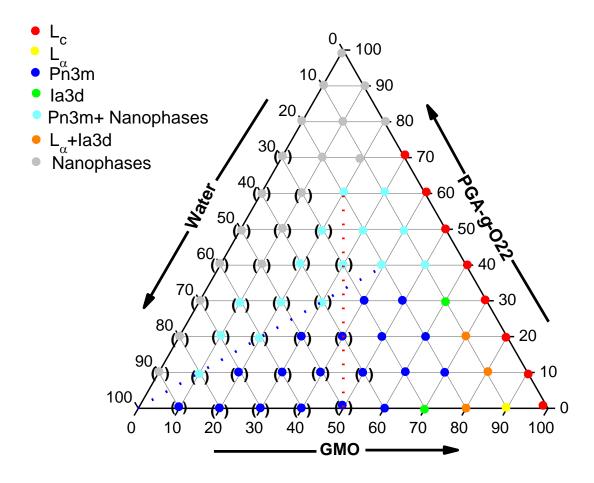


**Figure 3.7:** Differential scanning calorimetry traces of the PGA and the PGA-*g*-Ox recorded with a heating rate of 10 °C⋅min<sup>-1</sup>.

#### 3.3.3 The ternary system GMO/PGA-g-022/water

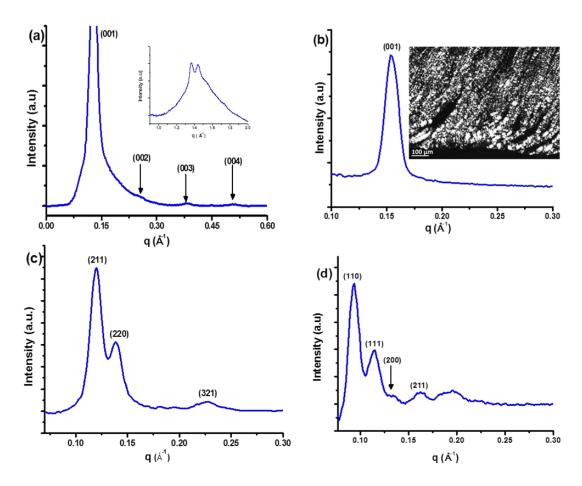
To identify various liquid crystalline phases, SAXS is employed and a detailed ternary phase diagram of GMO/PGA-*g*-Ox/water at 25 °C is constructed for one of the synthesized PGA-*g*-Ox, namely PGA-*g*-O22. This graft copolymer is selected since it has a similar volume ratio of oleate chains to polar polymer backbone (27 vol. %) as the volume ratio of the oleate chain to the glycerol polar head group in GMO (30 vol. %). The GMO/PGA-*g*-O22/water ternary phase diagram is depicted in Figure 3.8. If an excess of water is observed during preparation, this is indicated by brackets in the phase diagram.

Firstly, the focus is given to the behavior of the binary systems along the three axes (GMO-axis (GMO/water), PGA-g-O22-axis (GMO/PGA-g-O22), and water-axis (PGA-g-O22/water)) in the constructed ternary phase diagram. The GMO/water binary system has been studied in literature mainly in the range of large GMO contents.



**Figure 3.8.**Ternary phase diagram of the GMO/PGA-*g*-O22/water system at 25°C. The compositions in wt% indicates the feed ratios of the blends, while the brackets indicate those compositions where an excess of water is observed. The red dotted line indicates the direction of constant GMO/water ratio with varying PGA-*g*-O22 concentration whereas the blue dotted line. represents a constant GMO/PGA-*g*-O22 ratio with varying water concentration.

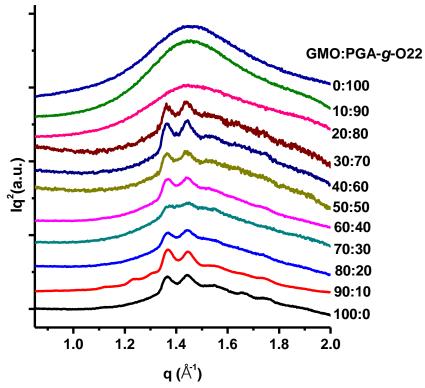
Figure 3.9(a) shows that GMO forms in bulk a lamellar crystal  $L_c$  phase with Bragg reflections observed by wide angle X-ray scattering (WAXS, see inset of Figure 3.9a). Upon increasing amounts of water, a liquid crystalline lamellar  $L_\alpha$  phase can be observed where the GMO molecules are arranged in bilayers separated by water channels and without Bragg reflections in the WAXS range. This is followed by a mixture of  $L_\alpha$  and the cubic la3d phase. The system GMO/water-70/30 exhibits exclusively the la3d phase and GMO/water-60/40 forms another cubic phase with Pn3m symmetry. At high water concentrations, the double diamond cubic phase of Pn3m symmetry remains existent with an excess of water of hydration which is in agreement with literature data. <sup>219,249,250</sup> The SAXS pattern of all discussed liquid crystalline phases are shown in Figure 3.9.



**Figure 3.9.** SAXS pattern at 25°C of (a) GMO/PGA-g-O22-80/20, (lamellar crystalline phase), the inset shows the scattering behavior in the WAXS regime, (b) GMO/water - 90/10, (liquid crystalline lamellar,  $L_{\alpha}$  phase), the inset shows its optical micrograph, (c) GMO/PGA-g-O22/water -60/30/10 (gyroid cubic phase with Ia3d symmetry), (d) GMO/PGA-g-O22/water - 60/10/30 (double diamond cubic phase of Pn3m symmetry). All the compositions are in wt%.

The PGA-g-O22 axis represents the binary blend system GMO/PGA-g-O22. Starting again with neat GMO it can be observed that with increasing amount of PGA-g-O22 the lamellar crystal  $L_c$  phase remains present up to the system GMO/PGA-g-O22-30/70 (see Figure 3.11b). The relative peak positions in the SAXS range of 1:2:3:4 etc. (for indexing see Figure 3.9) can be observed, and the typical Bragg reflections in the WAXS trace indicate again the formation of a crystalline phase (see Figure 3.10).

When the polymer content reaches 80 wt% in the system GMO/PGA-g-022 -20/80 the SAXS pattern is dominated of that by neat PGA-g-022 (cf. Figure 3.11b). The SAXS peak as a result of the nanophase separation of PGA-g-022 is not influenced by the presence of up to 20 wt% GMO. Thus, it can be concluded that the structure formation of neither GMO nor PGA-g-022 is influenced by the presence of the other compound significantly.

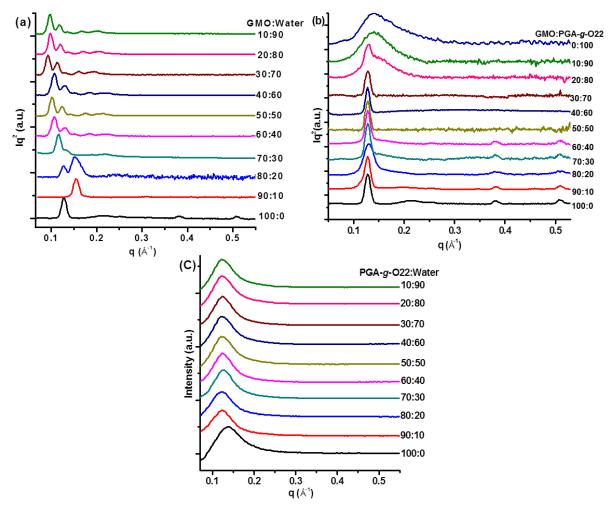


**Figure 3.10.** WAXS patterns of GMO/PGA-g-022 binary system.

The disappearance of the scattering peaks of the  $L_c$  phase of GMO, beyond GMO/PGA-g-O22-30/70 could be either due to the complete disintegration of the GMO microstructure due to higher polymer content or the insignificant contribution of GMO to the scattering due to its small content in the mixture.

The third binary system along the water-axis represents the binary system PGA-g-O22/water. As can be seen in Figure 3.11(c), the peak in the SAXS trace of PGA-g-O22 attributed to the nanophase separation of the oleate side chains into nanodomains within a matrix of the polar polymer backbone shifts to larger q-values when the water content in the blends is increased up to 20 wt% and remains constant upon further increase of the water content. This agrees with the observation that PGA-g-O22 swells in water but is not soluble in water. As given in Table 3.1, for dry PGA-g-O22, the average distance between the nanodomains is d = 48.2 Å calculated from the SAXS peak. With an increase of the water content to 20 wt%, the distance between the nanodomains increases slightly to approximately d = 52.3 Å caused by the swelling of the polar matrix. Higher amounts of water do not result in a further increase of the distance, but an excess of water can be detected.

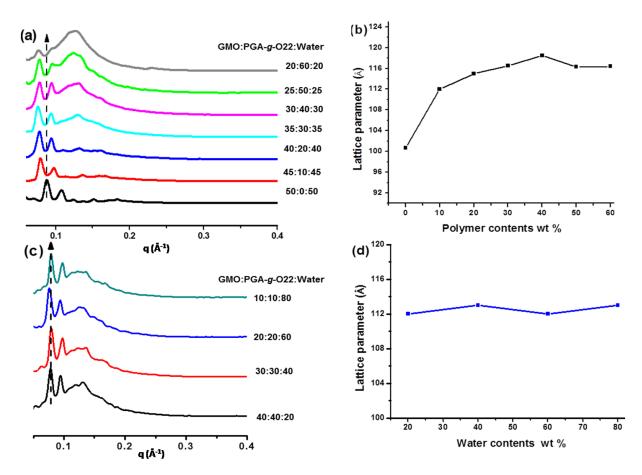
The presence of excess water, indicated by the brackets in Figure 3.8, can be detected in the full ternary phase diagram for all samples with at least 30 wt% of water, unless the amount of GMO exceeds the amount of water (i.e., left of the red dotted line in Figure 3.8). Swollen polymer, marked as 'nanophases' in Figure 3.8, is present in all samples with a polymer content greater than GMO (i.e., above the blue dotted line in Figure 3.8), only in case of water free samples, the behavior is different as described above.



**Figure 3.11:** SAXS patterns of binary systems at 25 °C of (a) GMO/water, (b) GMO/PGA-g-O22, and (c) PGA-g-O22/water. The corresponding compositions are given in wt%.

For samples with a higher GMO than polymer content, the same mesophase structures as in the neat GMO-water system (i.e., Pn3m, and Ia3d) can be observed, without an indication of a separate polymer phase. It can be assumed, that PGA-g-O22 is included to a certain extent in the GMO/water system. For example, the Ia3d morphology at GMO/water - 70/30 can also be found in the mixture of GMO/PGA-g-O22/water-60/30/10. In this case, almost all free water should be incorporated into the polymer, i.e. the swollen polymer substitutes the water in the gyroid cubic phase. However, with only

a partial substitution of water by the swollen polymer, the double diamond cubic phase with Pn3m symmetry is formed. This structure can be identified by the SAXS peak ratios of  $\sqrt{2}$ ,  $\sqrt{3}$ ,  $\sqrt{4}$ ,  $\sqrt{6}$ ,  $\sqrt{8}$ , according to the Pn3m symmetry for GMO/PGA-g-O22/water - 60/10/30. This morphology is also the most stable one when water or polymer exists in excess.



**Figure 3.12:** (a) SAXS profiles and (b) the respective lattice parameter of the Pn3m cubic phase of GMO/PGA-g-O22/water ternary systems with a constant GMO/water ratio while increasing the polymer content from 0 to 60 wt%. (c) SAXS profiles and (d) the respective lattice parameter with increasing water content from 20 to 80 wt% while keeping the GMO/PGA-g-O22 ratio constant at 1: 1.

As discussed above, GMO forms a liquid crystalline lamellar  $L_{\alpha}$  phase in the GMO/water binary system. Starting in this phase at GMO/ PGA-g-O22/water - 90/0/10, and keeping the total amount of water constant, the addition of polymer reduces by absorption the amount of available water, until at GMO/PGA-g-O22/water-60/30/10 almost all water is in the swollen polymer (Ia3d morphology). Between both points, a mixture of both phases,  $L_{\alpha}$  and Ia3d, can be observed. Further addition of polymer leads to an excess of a swollen polymer phase, and the Pn3m morphology is formed. This

transition is equivalent to that of the binary GMO/water system from low to high amounts of water. To obtain more information on the polymer incorporation into the cubic phases, various compositions, with a constant GMO/water ratio of 1:1 and increasing polymer content, and with the constant GMO/polymer ratio of 1:1 and increasing water content are investigated by SAXS.

Figure 3.12 (a) depicts the SAXS profiles of seven GMO/PGA-g-022/water systems, all with the same GMO/water ratio of 1:1 but with increasing polymer content from 0 to 60 wt%. The relative peak positions are  $\sqrt{2}$ ,  $\sqrt{3}$ ,  $\sqrt{4}$ ,  $\sqrt{6}$ ,  $\sqrt{8}$  according to the Pn3m space group of the cubic phase. The first peak maximum shifts towards lower q-values with increasing polymer content (shown by an arrow in Figure 3.12(a) which is a clear reflection of the cubic phase swelling due to the polymer insertion into the lipid bilayer. The corresponding lattice parameter, calculated according to Equation 3.2, is plotted as a function of polymer content in Figure 3.12(b). It increases significantly from approximately a = 101 Å in the absence of polymer to approximately a = 116 Å in the presence of 30 wt% PGA-g-022. At higher polymer contents, the lattice parameter remains almost constant and the polymer background scattering, however, becomes more dominant.

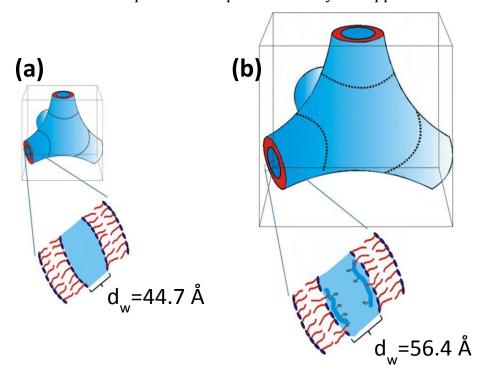
The water channels diameter of the cubic phase can be calculated from the geometry of the structure. $^{147,250}$  For GMO-water system with the Pn3m cubic phase the diameter of the water channel is given by equation 3.7.

$$d_w = 0.782a - 34.3 \,\text{Å} \tag{3.7}$$

At room temperature, the water channel diameter for the Pn3m cubic phases increased from 44.7 Å in the absence of PGA-g-O22 to approximately 56.4 Å with 30 wt% PGA-g-O22. Due to the identical chain structure of the oleate side chains of the PGA-g-O22 and the hydrophobic oleate tail of the GMO, it is assumed that the hydrophobic oleate side chains of the PGA-g-O22 penetrate the lipid bilayer while the PGA backbone, equipped with hydrophobic hydroxyl group and polar ester bonds, stays at the interface. The data show further that, the Pn3m cubic phase is stable and stays largely intact with increasing polymer content. In contrast, while keeping the ratio of GMO/PGA-g-O22 constant 1 : 1 while increasing the water amount from 20 to 80 wt% (Figure 3.12(c)), the lattice parameter of the Pn3m phase exhibits almost negligible changes as depicted in Figure 3.12(d), an indication of the fully swollen cubic phase state. By comparing the data of

Figure 3.12 (b) and 3.12 (d), it can be concluded that it is mainly the PGA-*g*-O22 content in the composition that controls the cubic phase swelling and the water channel enlargement.

The observation of the water channel enlargement and cubic phase swelling (cf. Figure 3.13), due to the addition of PGA-g-O22 to the GMO/water system, is very significant keeping in mind that mostly low molar mass additives, such as non-ionic octyl- $\beta$ -D-glucopyranoside ( $\beta$ -Glc-OC8)<sup>221</sup> and charged surfactant-doped systems dioctyl sodium sulfosuccinate (AOT)<sup>221</sup> neutral sucrose stearate,<sup>223</sup> charged lipids,<sup>222</sup> cholesterol,<sup>222</sup> and nucleic acids,<sup>224</sup> to name a few, have been observed to generate the cubic phase swelling and water channel enlargement. Furthermore, the addition of Pluronic® F127 to the GMO/water system has been found to transform the cubic phase symmetry from the double diamond Pn3m to the primitive Im3m that reflects the destabilization and disruption of the internal liquid crystalline structure.<sup>27,29,213</sup> The current study, however, signifies that amphiphilic grafted polymers, of a suitable design, could be a potential alternative and be exploited for tuning the behavior and properties of the lipid bicontinuous cubic phases for improved stability and applications.



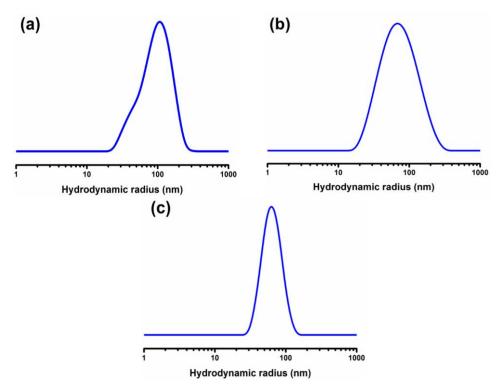
**Figure 3.13:** Schematic illustration of swelling of the Pn3m cubic phase. (a) Standard cubic phase from GMO/water - 50/50. (b) The swollen Pn3m cubic phase of the ternary system containing GMO/PGA-g-022/water - 30/40/30.

Additionally, PGA-*g*-Ox is biocompatible, biodegradable, and most important, in comparison to the traditional lower molar mass additives, the possibility of fine-tuning the behavior of PGA-*g*-Ox by structural adjustment with varying the hydrophobic/hydrophilic balance, molar mass, and the degree of grafting could open up a new avenue in material design for controlling the lipid liquid crystalline phase behavior and properties for enhanced biomedical and pharmaceutical applications.

# 3.3.4 PGA-g-022 as a potential stabilizer for GMO based nanoparticles in aqueous dispersions

As discussed above, the system GMO/water is frequently used to prepare cubosomes or other structured nanoparticles which usually require stabilization by Pluronic® type block copolymers.<sup>249</sup> The preceding results on the integration of PGA-g-O22 into the cubic phases formed by the GMO/water system led us to explore their potential application as a steric stabilizer of nanoparticles in aqueous dispersions. Employing the so-called interfacial deposition method, where the acetone solution of PGA-g-O22 and GMO, with calculated composition, is added slowly to water with regular vortexing for homogenization and evaporation of the acetone. The particle size in the resulting aqueous dispersion, determined by dynamic light scattering, is found to be  $R_h$  = 70 nm, 65 nm and 63 nm for PGA-g-O22, GMO/PGA-g-O22-90/10 and 80/20, respectively (see Figure 3.14).

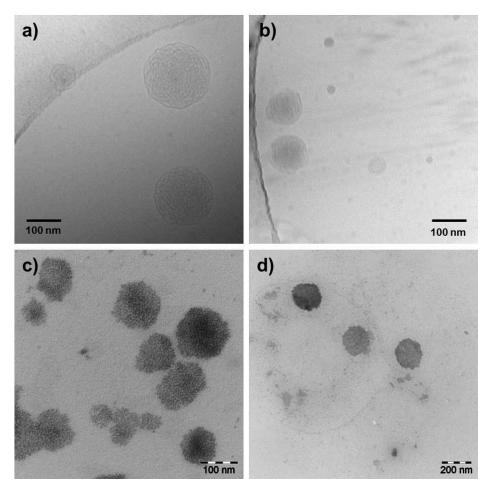
The formation of nanoparticles with an internal structure is visualized by cryo-TEM. The cryo-TEM images of the 1 wt% aqueous dispersions of GMO/PGA-*g*-022-90/10 (Figure 3.15(a)) and 80/20 (Figure 3.15(b)) reveal the formation of nanoparticles in the range of approximately 100 nm with well-defined internal structure. This is a strong indication that the synthesized amphiphilic graft copolymers could potentially be employed for the steric stabilization of internally structured nanoparticles in aqueous dispersion. The formation of nanoparticles is also verified by negative-stain TEM of a 0.2 wt% aqueous dispersion of GMO/PGA-*g*-022 - 90/10 as depicted in Figure 3.15(c). This image is in agreement with other negative-stain TEM images of cubosomes.<sup>251</sup> In contrast to cryo-TEM, negative-stain TEM is not able to show the internal structure of these nanoparticles since it is lost during the drying process of sample preparation.



**Figure 3.14**. Hydrodynamic radius distribution of (a) PGA-g-O22 (b) GMO/PGA-g-O22 - 90/10 (c) GMO/PGA-g-O22 - 80/20 in water at a concentration of 5 g·L<sup>-1</sup>, scattering angle of 90°, and at a temperature of 20°C.

The amphiphilic PGA-*g*-O22 copolymer could not be dispersed directly in water. However, the interfacial deposition method created a stable aqueous dispersion with self-assembled spherical nanoparticles as shown in the negative-stain TEM image (Figure 3.15(d)) of a 0.2 wt% aqueous dispersion of PGA-*g*-O22. In our previous studies on PGA grafted with stearate side chains (PGA-*g*-Sx), the formation of self-assembled nanoparticles, with well-defined structure due to phase separation that is driven predominantly by the crystallization of the saturated flexible stearate side chains, was observed.<sup>88</sup>

Due to the presence of the cis double bond, as discussed above, the oleate side chains cannot pack into a well-defined crystalline lattice and hence, PGA-g-Ox and the resulting nanoparticles are amorphous in nature. However, the amorphous nature of the PGA-g-Ox nanoparticles could be more useful and beneficial for pharmaceutical or other active ingredient delivery applications, as the crystallinity of the matrix has been found to have a significant influence on the drug loading and release rates. Generally, the amorphous matrix shows a higher capability of incorporating additives as compared with the crystalline matrix that often leads to expulsion of drugs.



**Figure 3.15:** Cryo-TEM images of 1 wt% aqueous dispersions of (a) GMO/PGA-*g*-022 -90/10 and (b) GMO/PGA-*g*-022 -80/20. TEM images of uranyl acetate stained 0.2 wt% dispersions of (c) GMO/PGA-*g*-022 - 90/10, and of (d) PGA-*g*-022.

#### 3.4 CONCLUSION

Amphiphilic graft copolymers with poly(glycerol adipate) (PGA) backbone and oleate side chains have been synthesized with various degrees of grafting, ranging from 11 to 90 mol%. The resulting PGA-g-Ox grafted polymers are amorphous in nature with phase separation of the oleate side chains into nanodomains. To evaluate the influence of the PGA-g-Ox on the mesophase behavior of the system glycerol monooleate (GMO)/water, a detailed ternary phase diagram of GMO/PGA-g-O22/water is constructed with the help of small angle X-ray scattering (SAXS) investigations. The addition of PGA-g-O22 to the GMO/water system, while maintaining a constant GMO/water ratio of 1: 1, induces swelling and enlargement of water channels in the inverse bicontinuous cubic phase. This is attributed to the integration of oleate side chains of the polymer into the lipid bilayers. Preliminary investigations reveal that the synthesized amphiphilic graft

polymers could potentially be used for the stabilization of the dispersed structured nanoparticles. In future, we shall study if different degrees of grafting of PGA-*g*-Ox could produce more robust cubic phase swelling of the system GMO/water with even more enlarged water channels.

### **Chapter 4**

#### 4 MULTIGRAFT POLYESTERS AS STABILIZERS FOR CUBOSOMES

#### 4.1 INTRODUCTION

As mentioned before, bicontinuous cubic lyotropic liquid crystalline phases are of significant interest because of the high interface to volume ratio, which makes them promising candidates for drug delivery system. In addition, they are used for *in-meso* crystallization of proteins for structure determination. Growing numbers of molecules are being synthesized that form inverse bicontinuous cubic phases,<sup>254,255</sup> however, lipids such as glycerol monooleate (GMO) and phytantriol are extensively used and studied.<sup>107,140,171,228,230,256-259</sup> When water is added to these lipids, a viscous gel-like cubic phase is formed. The high viscosity of cubic phases limits their application as they are difficult to handle. The easy solution to this problem is to break this bulk cubic phase into submicron particles called cubosomes.

Cubosomes are typically prepared by dispersing cubic phases of lipids or by dispersing homogeneous solutions of lipids in solvents like ethanol in water. Former methods need more energy (such as sonication). 182,249,260 However, both methods require the presence of steric stabilizer to avoid flocculation caused by van der Waals interactions. There are several molecules that can serve as steric stabilizers such as the PEG-stearate (Myrj-series),<sup>166,261</sup> PEGylated phospholipids, 186,262,263 series **PEGylated** monooleate,  $^{183,184}$  sorbitan monooleate (e.g., Tween 20, 40, 60 80),  $^{188,264}$  bile salts,  $^{265}$ amphiphilic proteins (albumin, β-casein), 182,266 and Pluronics®. However, Pluronic®F127 a triblock copolymer of PEG and PPO (PEG<sub>100</sub>PPO<sub>65</sub>PEG<sub>100</sub>) is being extensively used to stabilize cubosome dispersions because of its performance. 178,190,226,267-270 Chong et al. investigated a series of pluronics and discovered that Pluronic®F108 having longer PEG chains is even a better stabilizer than Pluronic®F127.<sup>178</sup> Besides linear block copolymers, graft copolymers can be used as steric stabilizers. The graft copolymers have low crystallinity, melting temperature, and CMC, so that they could better serve as steric stabilizers. There is not much work reported on the use of graft copolymers as steric stabilizers. Chong et al. have used the brush-like copolymer poly(octadecyl acrylate)*block*-poly(polyethylene glycol methyl ether acrylate) (P(ODA-*b*-P(PEGA-OME)) synthesized by reversible addition-fragmentation chain transfer (RAFT) polymerization, as a steric stabilizer of phytantriol and glycerol monooleate cubosomes. They found that phytantriol cubosomes stabilized with (P(ODA-*b*-P(PEGA-OME)) copolymers have a double diamond *Pn3m* cubic symmetry while cubosomes from GMO have primitive *Im3m* cubic symmetry.<sup>111</sup> There is always the need to introduce and investigate new materials to improve steric stabilization of lyotropic liquid crystalline dispersions.

Previously, enzymatically synthesized poly(glycerol adipate) was grafted with varying degree of oleate side chains, and their bulk properties were studied. In addition, a selected graft copolymer PGA-g-022 was further studied to investigate its effect on the mesophase behavior of the GMO-water system. From the ternary phase diagram of the PGA-*g*-022/GMO/water system, it was found that PGA-*g*-022 stabilizes the cubic Pn3m phase. For a high concentration of polymer the lattice parameter increased with increasing polymer concentration but the cubic symmetry retains.<sup>271</sup> These findings motivate us to further assess these graft polyesters for their ability towards steric stabilization of lyotropic liquid crystalline cubic dispersion (cubosomes). But these polymers are not water soluble to be used as a steric stabilizer directly. Therefore, a modification is required to make the polymer water soluble. The water solubility is typically achieved by adding a polymer with such properties as hydrophilicity, neutrality, the absence of hydrogen bond donors, the presence of hydrogen bond acceptors and it should have low toxicity and immunogenicity.<sup>272,273</sup> Poly(ethylene glycol) has all these features. Furthermore, the introduction of PEG chains to a polymer improves the pharmacokinetics and pharmacodynamics of drug delivery system (DDS).<sup>171</sup>

Poly(glycerol adipate)s with varying degrees of grafting of oleate and PEG side chains were synthesized to achieve a range of polymers with different hydrophilic to hydrophobic volume fractions. The properties of all synthesized graft copolymers were studied by <sup>1</sup>H NMR spectroscopy and gel permeation chromatography. The thermal properties are studied by differential scanning calorimetry. Furthermore, the ability of polymers as steric stabilizers of cubosomes was studied by visual assessment. The internal morphology was investigated by SAXS. The particle size of cubosomes was determined by dynamic light scattering (DLS). Scheme 4.1 describes the syntheses of the polymers under investigation

**Scheme 4.1:** Synthetic rout to (a) carboxylation of poly(ethylene glycol monomethyl ether), and (b) PEG and oleate grafted poly(glycerol adipate)(PGA<sub>x</sub>O<sub>y</sub>PEG<sub>z</sub>)

#### 4.2 EXPERIMENTAL PART

## 4.2.1 Materials

Glycerol, anhydrous THF, pyridine, *Candida antarctica* lipase B immobilized on acrylic resin commercially known as Novozym 435 (used after drying over P<sub>2</sub>O<sub>5</sub> for 24 h before use), succinic anhydride, oleoyl chloride and mPEG750 were purchased from Sigma Aldrich. N-(3-dimethylaminopropyl)-N-ethylcarbodiimide hydrochloride (EDC), chloroform, n-hexane, diethyl ether and methanol were purchased from Carl Roth. Divinyl adipate and mPEG1K was purchased from TCI-Europe. The glycerol monooleate used for this work was previously synthesized (see section 3.2.2.3) and is a mixture of G1MO (92

mol%) and G2MO (8 mol%). The PGA used for this work was synthesized as described by Kallinteri *et al.*<sup>83</sup> It has  $M_n$  of 5,300 g·mol<sup>-1</sup> and *PDI* of 1.9.

### 4.2.2 Syntheses

#### 4.2.2.1 Carboxylation of mPEG750 and mPEG1K

Carboxylation of poly(ethylene glycol) monomethyl ether (mPEG) was carried out as described by Lu *et al.* <sup>274</sup> with a small modification. In a typical experiment mPEG1K (10 g, 10 mmol) was added to a 250 mL three neck round bottom flask equipped with magnetic stirrer, heating plate and reflux condenser containing a CaCl<sub>2</sub> drying tube at its opening. 200 mL chloroform was added. After this, DMAP (0.122 g, 1 mmol) and succinic anhydride (2 g, 20 mmol) were added. The reaction was allowed to run for 24 h at 30°C. After this time, the reaction mixture was transferred into a separating funnel and the crude product was washed three times with brine solution. The organic phase was collected and dried by MgSO<sub>4</sub>. The crude product was recrystallized using ethyl acetate to have pure succinyl mPEG1K (mPEG1K-S). The purity was confirmed by <sup>1</sup>H NMR spectroscopy. (cf. Figure 4.1)

#### 4.2.2.2 Grafting of poly(glycerol adipate) (PGA) with oleate side chain

PGA used for the grafting with oleate has  $M_n$  = 5,300 g·mol<sup>-1</sup> and PDI = 1.9. PGA was grafted with oleate side chains according to the procedure described in section 3.2.2.2. Three types of oleate grafted PGAs were synthesized, i.e. PGA<sub>26</sub>O<sub>4</sub>, PGA<sub>26</sub>O<sub>7</sub>, and PGA<sub>26</sub>O<sub>13</sub>. The purity of the sample was confirmed by <sup>1</sup>H NMR spectroscopy. A representative spectrum of all three products PGA<sub>x</sub>O<sub>y</sub> is shown in Figure 4.1.

#### 4.2.2.3 PEG grafting of PGA<sub>26</sub>O<sub>x</sub>

Oleate grafted polymers are further grafted with PEG chains *via* esterification. In a typical experiment PGA<sub>26</sub>O<sub>4</sub> (1g, 4.08 mmol) was placed in a three neck 100 mL round bottom flask equipped with a septum and magnetic stirrer. The flask was placed in an ice bath. 60 mL chloroform was then charged into the reaction flask. A weighed amount of mPEG1K-S (0.9 g, 0.8 mmol), EDC (2.3 g, 12.2 mmol) and DMAP (0.15 g, 1.22 mmol) were then added. The ice bath was removed after 1 h and the reaction was allowed to run for 48 h at room temperature. After this time the reaction mixture was transferred into a separating funnel and washed 3 times with brine. The organic phase was dried with MgSO<sub>4</sub>, filtered and the solvent was evaporated

on a rotary evaporator. The crude product was further purified to remove un-reacted mPEG1K-S by dialysis in water using regenerated cellulose membrane having a cut off molar mass of 10 kDa for 7 to 10 days. After drying the solvent, the slightly yellowish solid product was obtained. The purity of the sample was confirmed by  $^{1}$ H NMR spectroscopy.  $^{1}$ H NMR (400 MHz, CDCl<sub>3</sub>):  $\delta$  5.37 – 5.28 (m, 2H), 5.24 (s, 1H), 4.36 – 4.24 (m, 5H), 4.21 (dd, J = 9.8, 4.9 Hz, 2H), 4.18 – 4.02 (m, 5H), 3.84 – 3.42 (m, 88H), 3.36 (s, 3H), 2.7-2.6 (m, 4H), 2.41-2.25 (m, 6H), 2.02-1.93 (m, 4H), 1.72 – 1.54 (m, 6H), 1.36 – 1.09 (m, 20H), 0.86 (t, J = 6.8 Hz, 3H).

#### 4.2.2.4 Polymer characterization

<sup>1</sup>H NMR spectra were recorded on a Varian Gemini NMR spectrometer at 400 MHz and 25°C in CDCl<sub>3</sub>. The number average molar mass  $M_n$ , weight average molar mass  $M_w$ , and polydispersity index  $M_w/M_n$  for polymer backbone and oleate grafted PGA were measured using ViscotekGPCmax VE 2001 with a column set CLM3008 (guard column) and 1GMHHR (analytical column) equipped with VE 3580RI refractive index detector using polystyrene standards and THF as the eluent with a flow rate of 0.1 mL·min<sup>-1</sup> at 22 °C (column temperature). For mPEG grafted polymers, the measurements were done with DMF with 0.01 M LiBr as mobile phase in a thermostated column oven kept at 80 °C. The calibration standards for the measurements were poly(methyl methacrylate) samples.

Differential scanning calorimetry (DSC) measurements were performed under nitrogen flow using a Mettler Toledo DSC 822e module. About 8-12 mg of the sample was filled in aluminum pans. For all measurements, the sample was first heated to  $T = 125 \, ^{\circ}\text{C}$  in order to remove the previous thermal history, and after holding this temperature for 5 min, they were cooled to  $T = -50 \, ^{\circ}\text{C}$  with the rate of  $10 \, ^{\circ}\text{C} \cdot \text{min}^{-1}$ . The samples were heated again to  $80 \, ^{\circ}\text{C}$  at  $10 \, ^{\circ}\text{C} \cdot \text{min}^{-1}$  to record their melting endotherm.

#### 4.2.2.5 Surface Tension Measurements

The surface tension  $\gamma$  of aqueous solutions of the polymers was measured as a function of polymer concentrations at 25°. Plotting  $\gamma$  versus polymer concentration (log C) yields the critical aggregation concentration (CAC) indicated by the intersection of the extrapolation of the two linear regimes where the curve shows an abrupt change in the slope (see Figure 4.5).

#### 4.2.2.6 XRD measurements

For XRD measurements, the cubic gel phase or cubosome dispersions were loaded into a capillary of 1.5 mm diameter. The capillary was sealed with epoxy resin on both sides. X-ray scattering experiments were performed in transmission mode using a SAXSLAB laboratory setup (Retro-F) equipped with an AXO microfocus X-ray source with an AXO multilayer X-ray optic (ASTIX) as a monochromator for Cu  $K_{\alpha}$  radiation ( $\lambda$ =0.154 nm). A DECTRIS PILATUS3 R 300K detector was used to record the two-dimensional scattering patterns. For cubic gel phase or cubosome dispersions the samples were loaded into a capillary of diameter 1.5 mm while for the bulk polymer, the sample holder is a 2 mm thick aluminum disc. The measurements were performed at room temperature for a q-range 0.25 - 7 nm<sup>-1</sup> for the cubic gel phase or cubosome dispersions. For the measurements of bulk polymer a q-range of 0.25 - 7 nm<sup>-1</sup> and 1 - 29 nm<sup>-1</sup> to cover the small and wide angle scattering range respectively.

#### 4.2.2.7 Dynamic light scattering

DLS measurements were performed using an ALV/DLS-5000 instrument (ALV GmbH, Langen, Germany). As a light source, a 20 mW He–Ne gas laser (632.8 nm, 20 mW) was used (Uniphase Laser, Palo Alto, California). The DLS instrument was equipped with a goniometer for automatic measurements between scattering angles  $\theta$  of 30 and 90°. The correlation functions were analyzed by the CONTIN method, which gives information on the distribution of decay rates  $\Gamma$ . Apparent diffusion coefficients were obtained from  $D_{app} = \Gamma/q^2$  (where  $q = (4\pi n/\lambda) \sin(\theta/2)$ ,  $\lambda$  is the wavelength of the light, n is the refractive index, and  $\theta$  is the scattering angle). Finally, apparent hydrodynamic radii were calculated via the Stokes–Einstein equation.

$$R_h = \frac{k_B T}{6\pi \eta D_{app}} \tag{4.1}$$

Where,  $k_B$  is the Boltzmann constant and  $\eta$  is the viscosity of the solvent at temperature T.

#### 4.2.3 Preparation of cubosome dispersions

Cubosome dispersions were prepared, using a top-down approach. A weighed amount of GMO was taken in an Eppendorf tube. During heating the sample to 50°C GMO was melted. A calculated amount of 2 wt% of stabilizer solution was added to achieve 1,

3, 5, and 10 wt% of GMO and mixed with strong spatulation to obtain the cubic gel phase also known in literature as the bulk cubic phase.<sup>249,275-277</sup> The samples were further diluted with distilled water and homogenized using silentCrusher S for 15 min with a break of 1 min at a speed of 45,000 rpm after every 1.5 min mixing to provide 10 wt% (of combined mass of GMO and stabilizer) dispersions.

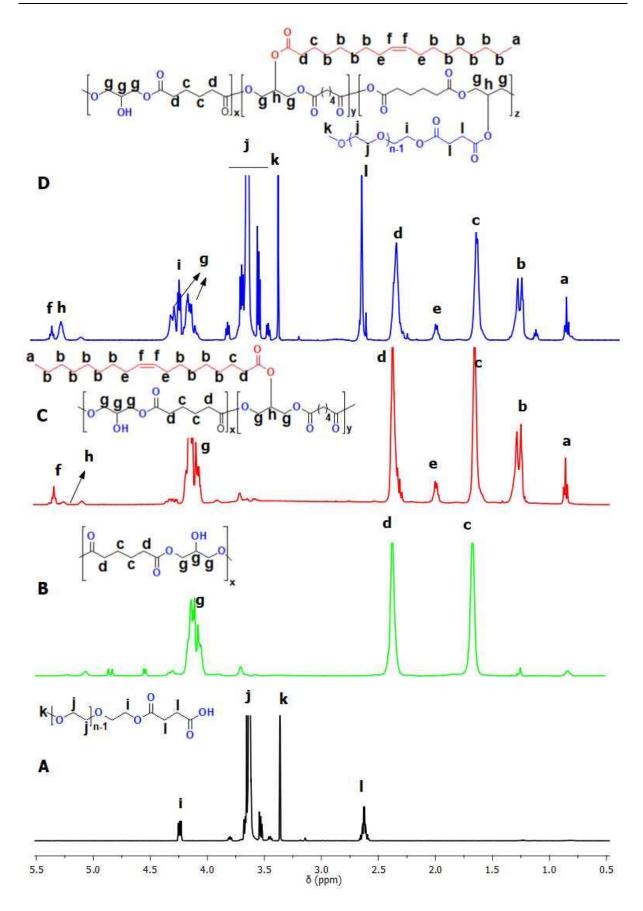
#### 4.3 RESULTS AND DISCUSSION

## 4.3.1 Polymer synthesis and grafting

Poly(glycerol adipate) was successfully synthesized using CAL-B catalyzed polycondensation reaction. The reaction was carried out at 50°C. Since enzymes are regioselective to a great extent, as only 4% branching was observed<sup>271</sup> under this reaction condition, so a linear poly(glycerol adipate) is obtained. As discussed before, a steric stabilizer must have a hydrophobic part that could anchor to the lipid bilayer. <sup>171</sup>

For this work, oleic acid is selected as a hydrophobic chain, which is also part of GMO. The grafting of PGA with oleate chains was carried out by simple esterification of activated acid and pendant –OH groups of the polymer backbone using pyridine as an acid scavenger. Oleate grafted poly(glycerol adipate) was further grafted with mPEG chains. For this purpose mPEG was reacted with succinic anhydride catalyzed by DMAP. The succinyl mPEG was grafted to the polymer backbone by simple esterification reaction using EDC as a coupling agent in the presence of DMAP. Graft copolymers with different degrees of oleate side chains and mPEG chains were synthesized. The variation in grafting yields polymers with different hydrophilic to lipophilic balance, which is an important factor in order to understand the stabilization ability of graft copolymers. The graft copolymers are represented by PGA<sub>x</sub>O<sub>y</sub>PEG<sub>z</sub>, where *x* is the degree of polymerization of PGA, *y* stands for the number of oleate side chains connected to the polymer backbone, whereas *z* stands for number of grafted PEG chains.

The syntheses of the graft copolymers were confirmed by  $^1H$  NMR spectroscopy. A representative spectrum of carboxylated mPEG, PGA<sub>x</sub>, PGA<sub>x</sub>O<sub>y</sub>, and PGA<sub>x</sub>O<sub>y</sub>PEG<sub>z</sub> are shown in Figure 4.1.



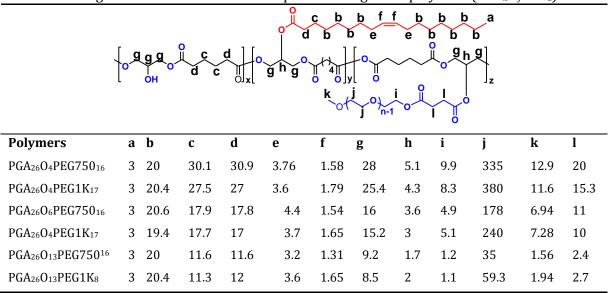
**Figure 4.1:**  $^{1}$ H NMR spectrum of (A) mPEG1K-S, (B) PGA<sub>26</sub>, (C) PGA<sub>26</sub>O<sub>4</sub>, (D) PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> recorded at 27  $^{\circ}$ C using CDCl<sub>3</sub> as a solvent.

All the peaks are very well assigned, indicating the purity of the products. The integral values of all the grafted polymers are given in Table 4.1. The degree of grafting of oleate side chains and mPEG side chains is calculated by equations 4.2 and 4.3, respectively, using integral values of the <sup>1</sup>H NMR spectrum of a particular product.

mol% oleate chain grafting = 
$$\frac{1.33 \times a}{d - 0.67a} \times 100$$
 (4.2)

$$mol\% \ mPEG \ grafting = \frac{k}{g+h} \times \frac{5}{3} \times 100$$
 (4.3)

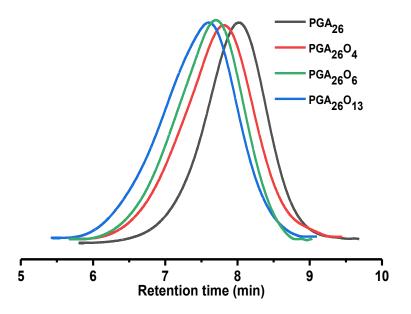
Table 4.1: Integral values from the <sup>1</sup>H NMR spectra of all grafted polymers (PGA<sub>x</sub>O<sub>y</sub>PEG<sub>z</sub>).



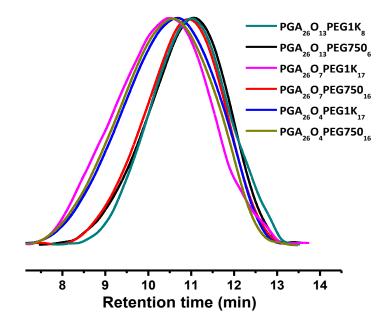
All the synthesized polymers are further characterized by gel permeation chromatography. Because DMF is not a good solvent for oleate grafted polymers, the GPC measurements of PGA and oleate grafted PGAs were carried out in THF.

The GPC traces of PGA and oleate grafted PGA are shown in Figure 4.2. In the figure 4.2 a successive shifting of the peak to the higher molar mass confirms the grafting reaction. GPC traces of all graft copolymer samples  $PGA_xO_yPEG_z$  are shown in Figure 4.3. From the analysis of these chromatograms, it is noticed that the PDI of some of the oleate grafted polymers increased after grafting with mPEG chains instead of decreasing. This could be a sign of hydrolytic cleavage of the ester bond. Since the removal of unreacted mPEG-S chains was difficult, the products were dialyzed with water for 7 to 10 days. The exposure of the product to water for such a long time might lead to cleavage of ester links.

However, this hydrolytic cleavage is not very big as all the products have symmetric and unimodal molar mass distributions.



**Figure 4.2:** GPC traces of PGA and oleate grafted PGA, measured in THF, against polystyrene standards at temperature 22°C.

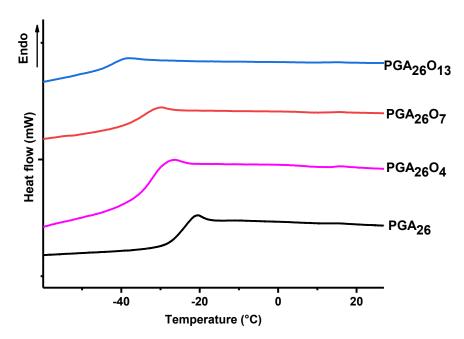


**Figure 4.3:** GPC traces of all grafted polymers  $PGA_xO_yPEG_z$  measured in DMF with 0.01 M LiBr as eluent at 25°C.

The thermal properties of all the polymers were determined by differential scanning calorimetry. It was observed that the polymer backbone (PGA) and all oleate grafted polymers are amorphous since a melting peak from these polymers is not observed.

1.

However, a glass transition temperature was observed that decreases with increasing degree of grafting which is consistent with previous findings (see Table 4.2.).<sup>271</sup> The DSC traces of PGA and  $PGA_xO_y$  are shown in Figure 4.4.



**Figure 4.4**: DSC traces of PGA and oleate grafted PGA recorded at a heating rate of 10°C⋅min-

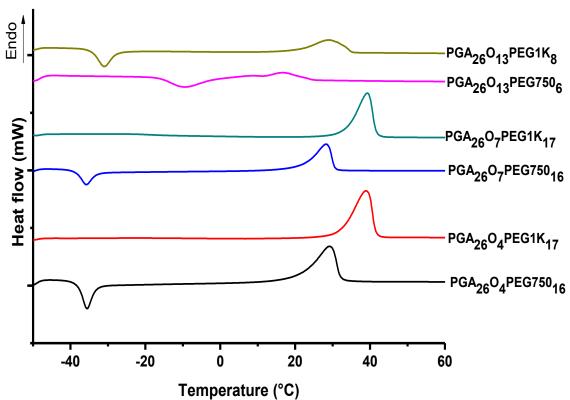
The oleate grafted PGAs are then further grafted with mPEG750 and mPEG1K side chains. The DSC traces of mPEG grafted  $PGA_xO_y$  are shown in Figure 4.5. It is observed that after grafting with PEG side chains, all the polymers become semi-crystalline.

The phenomenon of cold crystallization was also observed in some samples where the volume fraction of PEG is relatively small.<sup>278</sup> The cold crystallization temperature of the prodcuts PGA<sub>26</sub>O<sub>4</sub>PEG750<sub>16</sub>, PGA<sub>26</sub>O<sub>7</sub>PEG750<sub>16</sub>, PGA<sub>26</sub>O<sub>13</sub>PEG750<sub>6</sub>, and PGA<sub>26</sub>O<sub>13</sub>PEG1K<sub>8</sub> is -35.6, -35.9, -9.4 and -30.8 °C, respectively. The reason of this cold crystallization is that in these sample during the cooling step the chains do not have enough time to organize themselves as the mobility is hindered by neighboring chains. So during the heating scan, they organize themselves and achieve an ordered state.<sup>278,279</sup> The melting temperatures  $T_m$ , glass transition temperatures  $T_g$ , crystallinity, number average molar masses  $M_n$  and polydispersity index PDI of all graft copolymers are given in Table 4.2.

The crystallinity of the graft copolymers was calculated by the following relation,

$$X = \frac{\Delta H_m}{\Delta H_m^0 \cdot W_{PEG}} \tag{4.4}$$

Here,  $w_{PEG}$  is the mass fraction of PEG chains in the graft copolymer,  $\Delta H_m$  is the melting enthalpy of the corresponding PEG chains in the polymer,  $\Delta H_m^0$  is the melting enthalpy of 100% crystalline PEG. The value of  $\Delta H_m^0$  is 197 J·g<sup>-1</sup>.<sup>280</sup>



**Figure 4.5**: Differential scanning calorimetry traces of graft copolymers ( $PGA_xO_yPEG_z$ ) recorded at a heating rate of  $10^{\circ}C\cdot min^{-1}$ .

It is worth mentioning here, that the crystallinity in graft copolymers is induced by PEG chains as the PGA and oleate grafted PGA are amorphous materials. SAXS and WAXS scans of the bulk polymer are shown in Figure 4.6. A typical pattern of a lamellar crystal phase in the SAXS region and the characteristic pattern of PEG in the WAXS region respectively confirm that the crystallinity is induced by PEG chains.

Figure 4.6(a) shows the SAXS pattern of the bulk polymer  $PGA_{26}O_4PEG1K_{17}$ . It depicts the presence of the lamellar arrangement, as periodic lamellar peaks are present. The first order lamellar peak appears at q=0.0513 Å<sup>-1</sup> with the corresponding d-spacing of 47.9 Å at 25°C. The lamellar thickness value is calculated as 36 Å by considering the

crystallinity of the polymer (X=67%) obtained from DSC. By increasing the temperature, peaks slightly shift to lower q-values due to the increase of lamellar thickness.<sup>281</sup>

**Table 4.2:**  $M_n$ , PDI,  $\phi_{oleate}$ ,  $\phi_{mPEG}$ ,  $T_g$ , and  $T_m$  of all grafted and ungrafted polymers.

Polymer	M <sub>n</sub> (g·mol·  1)	PDI	$\phi_{oleate}{}^{ m d}$	$oldsymbol{\phi}_{PEG^{ extbf{d}}}$	Т <sub>д</sub> е (°С)	T <sub>m</sub> e	Crystallinitye (%)
PGA <sub>26</sub>	5,300a	1.9a	-	-	-24	-	-
PGA <sub>26</sub> O <sub>4</sub>	6,350 <sup>b</sup>	1.7a	18	-	-33	-	-
PGA <sub>26</sub> O <sub>7</sub>	7,250 <sup>b</sup>	2.0a	0.28	-	-35	-	-
PGA <sub>26</sub> O <sub>13</sub>	8,750b	1.9a	0.42	-	-42	-	-
PGA <sub>26</sub> O <sub>4</sub> PEG750 <sub>16</sub>	19,900 <sup>b</sup>	2.7c	0.07	0.64	-	29.2	61
PGA <sub>26</sub> O <sub>4</sub> PEG1K <sub>17</sub>	25,000b	1.8c	0.05	0.73	-	38.9	67
PGA <sub>26</sub> O <sub>7</sub> PEG750 <sub>16</sub>	20,700 <sup>b</sup>	1.8c	0.1	0.62	-	28.4	52
PGA <sub>26</sub> O <sub>7</sub> PEG1K <sub>17</sub>	25,800 <sup>b</sup>	2.4 <sup>c</sup>	0.08	0.71	-	39.2	66
PGA <sub>26</sub> O <sub>13</sub> PEG750 <sub>6</sub>	13,800 <sup>b</sup>	1.9c	0.28	0.33	-	17	32
PGA <sub>26</sub> O <sub>13</sub> PEG1K <sub>8</sub>	17,500 <sup>b</sup>	2.1 <sup>c</sup>	0.22	0.47		29	53

<sup>&</sup>lt;sup>a</sup> Obtained from GPC using THF as eluent

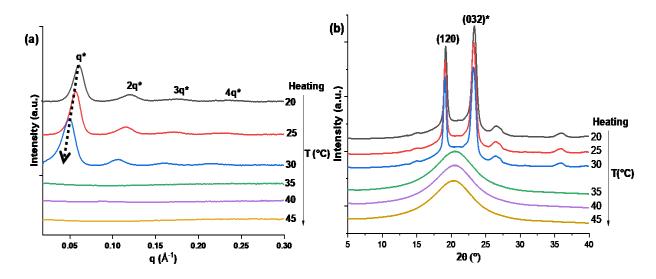
In Figure 4.6(b) the WAXS pattern of the polymer is shown with the presence of characteristics peaks of PEG until melting which corresponds to the typical triclinic crystal structure.<sup>282</sup> The peak vanishes by increasing the temperature which confirms that the crystallinity in the polymer was induced by PEG chains.

 $<sup>^{\</sup>mathrm{b}}$  Calculated on the basis of the degree of grafting obtained from  $^{1}\mathrm{H}$  NMR spectra

<sup>&</sup>lt;sup>c</sup> Obtaind from GPC, using DMF (with 0.01M LiBr) as eluent

<sup>&</sup>lt;sup>d</sup> Calculated from material studio software v 4.1

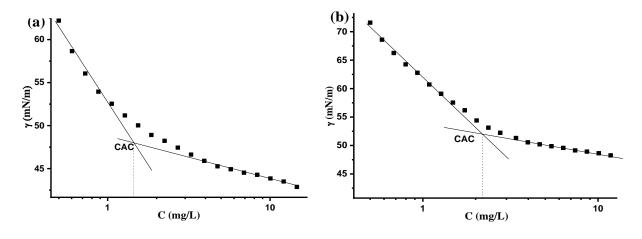
 $<sup>^{\</sup>text{e}}$  Obtained from DSC with a heating rate of  $10^{\circ}\text{C}{\cdot}\text{min}^{\text{-}1}$ 



**Figure 4.6:** (a) SAXS and (b) WAXS patterns of the bulk polymer  $PGA_{26}O_4PEG1K_{17}$  measured for different temperatures.

## 4.3.2 Graft copolymers as steric stabilizers of cubosomes

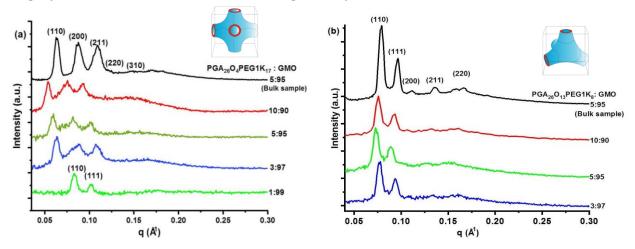
Out of all synthesized graft copolymers, only two polymers  $PGA_{26}O_4PEG1K_{17}$  and  $PGA_{26}O_{13}PEG1K_8$  were used further to investigate their properties as steric stabilizers for lyotropic liquid crystalline particles. The reason behind the selection of these polymers is that they have comparable volume fraction of PEG chains but differ in the volume fraction of oleate chains.



**Figure 4.7:** Surface tension of (a)  $PGA_{26}O_4PEG1K_{17}$  and (b)  $PGA_{26}O_{13}PEG1K_8$  in water as a function of polymer concentration at 25 °C.

The basic requirement for a steric stabilizer is that it must be water soluble and has a low critical aggregation concentration. The polymers mentioned fulfill both requirements. The CAC values for these polymers are obtained from tensiometry where

an increase in polymer concentration causes a decrease in surface tension of the aqueous solutions (see Figure 4.7). The CAC values are calculated to 1.45 and 2.2 g·L<sup>-1</sup> for the polymers P1 and  $PGA_{26}O_{13}PEG1K_8$ , respectively.



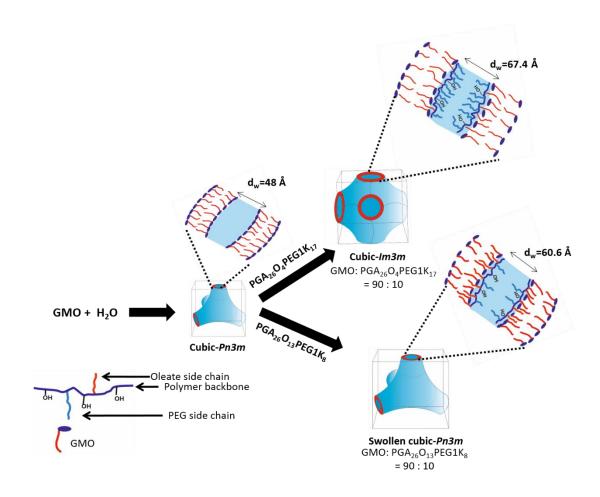
**Figure 4.8:** SAXS pattern of cubosomes samples stabilized by (a)  $PGA_{26}O_4PEG1K_{17}$  and (b)  $PGA_{26}O_{13}PEG1K_8$  measured at room temperature. Aqueous dispersions of GMO plus stabilizer at 10 wt% concentration were used for measurements. Curves in black correspond to the non-dispersed cubic phase.

For cubosome preparation for SAXS measurement, 1, 3, 5, and 10 wt % of each stabilizer with respect to GMO were used. Aqueous dispersions of GMO plus stabilizer at 10 wt% concentration were used for measurements. As reported before, GMO in excess water shows a Pn3m cubic phase. The GMO/water cubic phase could only incorporate as much as 1 wt% of PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub>. Increasing the concentration of PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> to more than 1 wt% leads to a change of the cubic symmetry from the cubic Pn3m to the cubic Im3m. (see Figure 4.8).

The lattice parameter of the Im3m cubic phase increases with increasing polymer concentration from 142 Å to 166 Å (with an increase in the diameter of the water channel from 48 to 67.4 Å). It is interesting to note that the lattice parameter of cubosomes is only slightly greater than in the non-dispersed cubic phase for the same ratio of polymer to GMO.

In comparison to  $PGA_{26}O_4PEG1K_{17}$ , when  $PGA_{26}O_{13}PEG1K_8$  is used as a steric stabilizer, surprisingly it retains the cubic Pn3m symmetry in all tested samples. The lattice parameter of the Pn3m cubic phase increases from 115.3 to 121.5 Å (the diameter

of the water channel increase from 48 to 60.6 Å) when the polymer  $PGA_{26}O_{13}PEG1K_8$  concentration increases from 3 wt% to 10 wt%. The lattice parameter of the cubic Pn3m phase is 107 Å for the GMO-water system ( $d_W$  = 48 Å). It is important to mention here that the sample with 1 wt% of  $PGA_{26}O_{13}PEG1K_8$  also shows a cubic Pn3m phase, but with this amount of stabilizer, only a small amount of GMO is possible to disperse which is not sufficient for SAXS measurement.

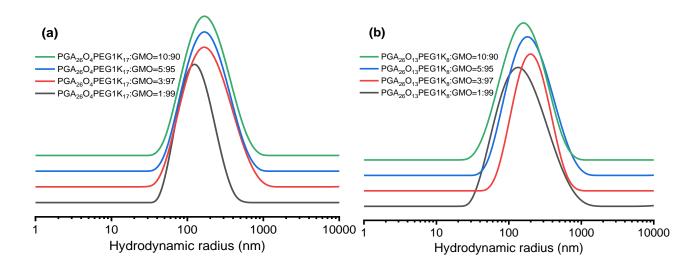


**Figure 4.9.** Schematic illustration of phase transition and swelling of cubic phases when polymer  $PGA_{26}O_4PEG1K_{17}$ , and  $PGA_{26}O_{13}PEG1K_8$  were used as steric stabilizers for cubosome dispersions.

The two polymers behave differently when added to the GMO/water system. As the polymer  $PGA_{26}O_4PEG1K_{17}$  induces a cubic phase transition from Pn3m to Im3m, in contrast, the  $PGA_{26}O_{13}PEG1K_8$  polymer retains the cubic Pn3m symmetry. The transition from the Pn3m cubic phase to the Im3m cubic phase indicates that the excess  $PGA_{26}O_4PEG1K_{17}$  molecules, which were saturated at the surface of the cubic phase, are incorporated with GMO and consequently formed the Im3m cubic phase. This could be further explained by taking into account the critical packing parameter. The mesophase

transition could only be observed in the less curved phase (i.e the Im3m cubic phase) when an amphiphile with a larger hydrophilic part compared to hydrophobic part  $\gamma$ <1 was added. $^{109,122}$  On the contrary, when the polymer PGA26O13PEG1K8 which is less hydrophilic than PGA26O4PEG1K17 is used as stabilizer, the hydrophobic side chains penetrate into the lipid bilayer, while the hydrophilic part remain at the interface. This results in an increase of the lattice parameter from 107.1 to 121.6 Å (hence an increase in the diameter of the water channel from 48 to 60.6 Å) of the cubic Pn3m phase. A schematic overview of the cubic phase transition and the cubic phase swelling when polymer PGA26O4PEG1K17 and PGA26O13PEG1K8 are used as stabilizers is shown in Figure 4.9.

To find out the particle size of the cubosomes, the samples were diluted to make 2 g·L·¹ concentrations for DLS measurement. The dilution is necessary in order to minimize undesired multiple scattering effects and, furthermore, to minimize interparticle interactions. The particle size was determined for each sample for 7 different angles (see Figure A5 and A6 in the Appendix). The average hydrodynamic radius of all measured sample varies from 130 nm to 225 nm and the hydrodynamic radius distributions for each sample measured at an angle of  $90^{\circ}$  is shown in Figure 4.10.



**Figure 4.10:** The hydrodynamic radius distribution of all cubosome samples stabilized by polymer  $PGA_{26}O_4PEG1K_{17}$  and  $PGA_{26}O_{13}PEG1K_8$  in different ratios with respect to GMO measured at a scattering angle of  $90^\circ$ . The concentration of the samples was  $2 \text{ g} \cdot \text{L}^{-1}$ .

The cubosome dispersions stabilized with polymers  $PGA_{26}O_4PEG1K_{17}$  and  $PGA_{26}O_{13}PEG1K_8$  are stable for more than 2 weeks. The stability of dispersions was identified by visual inspection, as no large aggregates were observed.

#### 4.4 Conclusion

PEG grafted poly(glycerol adipate)-g-oleate PGA<sub>x</sub>O<sub>y</sub>PEG<sub>z</sub> is synthesized by esterification reactions of oleate and PEG chains to the PGA backbone. DSC measurements showed that the graft copolymes are semicrystalline. The crystallinity was induced by the PEG chains. In some copolymyers where the volume fraction of PEG is relatively small  $(\phi_{PEG} \le 0.64)$  the phenomenon of cold crystallization was observed. All the PGA<sub>x</sub>O<sub>y</sub>PEG<sub>z</sub> samples were water soluble. Two of the selected polymers, PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> and PGA<sub>26</sub>O<sub>13</sub>PEG1K<sub>8</sub> having CAC values of 1.45 and 2.2 g·L<sup>-1</sup>, respectively, were used to investigate their ability as steric stabilizers of cumbosomes. It was found that the incorporation of PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> to GMO-water system causes a mesophase transition of the cubic phase from Pn3m to Im3m. On the contrary, when PGA26O13PEG1K8 was introduced into the GMO-water system, *Pn3m* cubic symmetry retained. It is assumed that the polymer PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> has a higher volume fraction of the hydrophilic part ( $\phi_{PEG}$  = 0.73) in comparison to the polymer PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> ( $\phi_{PEG} = 0.47$ ). Hence, when it interacted with the lipid bilayer, it increased the volume of head the group leading to cubic phase transition from *Pn3m* to *Im3m*. The polymer PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> retained the cubic symmetry of *Pn3m* and caused only an increase of the lattice parameter and thus of the radius of the water channels. The cubosome dispersions were stable for more than two weeks at room temperature. From these findings, it was concluded that these multi-graft biocompatible copolymers could be effectively used to stabilize several lyotropic liquid crystal systems by controlling the hydrophobic to hydrophilic volume fractions.

Chapter 5 Summary

## **CHAPTER 5**

#### **5 SUMMARY**

The enzymatic synthesis of functional polyesters is the most effective way to obtain them without product contamination with heavy metals. It is especially useful when biobased monomers are used for polymerization as reduced sugars e.g. xylitol and D-sorbitol. The direct esterification of such monomers can result in hyperbranched or crosslinked products. In the first part of this work, linear sugar-based polyesters such as poly(xylitol adipate) and poly(D-sorbitol adipate) of molar masses 5,000 and 3,500 g·mol¹, respectiely, were successfully synthesized. These are amorphous polymers and they are highly viscous liquids at room temperature. These polymers are biodegradable with great potential for the application in drug delivery system. The free pendant OH groups of the polymer backbone provide the possibility for further modification to achieve desired properties.

By esterification of hydroxyl groups on the polymer backbone with a saturated fatty acid such as stearic acid, a range of amphiphilic polyesters with different degree of hydrophilic-lipophilic balance are obtained. The study on the bulk properties of these comb-like amphiphilic polymers reveals that all the grafted polymers are semi-crystalline. The crystallinity arises from the immiscibility of the grafted chains with the polymer backbone. Small angle X-ray scattering data show a typical lamellar ordering while the wide-angle X-ray scattering pattern shows a short range order which is a typical hexagonal rotator phase. Furthermore, the self-assembly behavior of these amphiphilic polyesters was studied by negative staining TEM and dynamic light scattering. Stearoyl grafted poly(C)-sorbitol adipate) shows spherical self-assemblies whereas stearoyl grafted poly(D-sorbitol adipate) forms nanoparticles with a unique structure. It would be interesting, in the future, to explore the morphology and the hydrolytic stability of the nanoparticles formed from these polymers. This is important for the application of these polymers in drug delivery system. Due to the biodegradability of these nanoparticles, they might be an alternative to many Pluronic® based systems.

Previously, intensive work has been done on poly(glycerol adipate) grafted with saturated fatty acids of variable lengths such as lauric acid, stearic acid behenic acid.

Chapter 5 Summary

However, not much is known about the graft copolymers, when an unsaturated fatty acid is grafted to the polyester backbone. The second part of this work deals with the synthesis and grafting of poly(glycerol adipate) with oleate side chains. Differential scanning calorimetry of all grafted and ungrafted polyesters demonstrates that all the polymers are amorphous having glass transition temperatures which decrease from -24 °C (for ungrafted) to -67 °C (for highest grafted polymers). Although, all the oleate grafted PGAs are amorphous, but X-ray diffraction analysis reveals a broad peak in the small angle regime with *d*-spacing values decreasing with increasing degree of grafting. It is assumed that the broad peak is the result of nanophases separation of oleate side chain from the polymer backbone. Furthermore, one of the selected polymers PGA-g-022 was chosen to study the effect of this polymer on the mesophase behavior of the glycerol monooleate/water system. A ternary phase diagram based on PGA-g-022/GMO/water was established. From the ternary phase diagram, it is clear that the polymer stabilizes the *Pn3m* cubic phase over a wide range of concentrations. There is a significant increase of the lattice parameter with an increase in polymer concentration. This increase of the lattice parameter is attributed to the widening of lipid bilayer and the water channels of the cubic phase. Later, this oleate grafted polymer was used to stabilize cubosomes. But the polymer is too hydrophobic to be effectively used as a steric stabilizer of cubosomes. So there is a need to modify this polymer to introduce a more hydrophilic character.

The last part of this work deals with the modification of oleate grafted poly(glycerol adipate) with a hydrophilic polymer such as poly(ethylene glycol) and studying the bulk properties of these polymers as well as their ability to stabilize cubosome dispersions. For this study three oleate grafted poly(glycerol adipate)s were further grafted with mPEG750 and mPEG1K chains. All the PEG-grafted polyesters are semi-crystalline. SAXS measurements depict a lamellar morphology in the small angle scattering regime, while WAXS measurements show a typical scattering pattern of the triclinic unit cell of PEG. All the PGA<sub>x</sub>O<sub>y</sub>PEG<sub>z</sub> samples are water soluble. Two polymers PGA<sub>26</sub>O<sub>4</sub>PEG1K<sub>17</sub> and PGA<sub>26</sub>O<sub>13</sub>PEG1K<sub>8</sub> having CAC values of 0.028 and 0.151 g·L·¹, respectively, were used to investigate their ability as steric stabilizers of cumosomes. It was found that adding the former ( $\phi_{PEG}$ =0.71) to the GMO/water system induces a mesophase transition of the cubic phase from Pn3m phase to the less curved Im3m cubic symmetry whereas the later ( $\phi_{PEG}$ =0.47) retains the cubic symmetry to the Pn3m with increased lattice parameter. The increase of the lattice parameter of the cubic phase is attributed to the penetration of

Chapter 5 Summary

hydrophobic chains into the lipid bilayer. The cubosome aqueous dispersions are stable for more than two weeks at room temperature. So, these multi-graft biodegradable copolymers could be effectively used to stabilize several lyotropic liquid crystal systems by controlling the hydrophobic to hydrophilic volume fractions.

Overall it has been shown that functional polyesters offer an interesting toolbox for the preparation of various biodegradable materials. In order to tailor their properties, not only different fatty acids with different grafting densities can be used but also other hydrophilic side chain can be employed to control the hydrophilic to lipophilic balance. The polymer backbones can be used for direct coupling of drugs, proteins and peptides.

Some of the chapters of this thesis are based on the following publications:

Chapter 2 based on

Bilal, M. H.; Prehm, M.; Njau, A.; Samiullah, M.; Meister, A.; Kressler, J. Enzymatic Synthesis and Characterization of Hydrophilic Sugar Based Polyesters and Their Modification with Stearic Acid. Polymers 2016, 8, 80.

Chapter 3 based on

Bilal, M. H.; Hussain, H.; Prehm, M.; Baumeister, U.; Meister, A.; Hause, G.; Busse, K.; Mäder, K.; Kressler, J. Synthesis of Poly(Glycerol Adipate)-*g*-Oleate and Its Ternary Phase Diagram with Glycerol Monooleate and Water. Eur. Polym. J. 2017, 91, 162–175.

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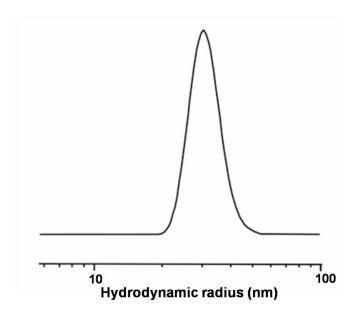
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## 7 APPENDIX



**Figure A1.** Hydrodynamic radius distribution of PXA at concentration 10 g·L $^{-1}$  at temperature 25 °C.

**Table A1.** WAXS data of PXA-*g*-S15.

T (°C)	q (A <sup>-1</sup> )	d (Å)	
30 °C heating	1.3663	4.599	diffuse
0	1.5222	4.128	$q_{\mathrm{w}}$
70 °C	1.3817	4.547	diffuse
30 °C cooling	1.4138	4.444	diffuse
	1.5204	4.133	$q_{\mathrm{w}}$

**Table A2**. SAXS data of PXA-*g*-S15.

T (°C)	q (A <sup>-1</sup> )	d (Å)	
30 °C heating	0.1136	55.310	q *
70 °C ⊂	0.1284	48.934	<b>Broad Peak</b>
30 °C cooling	0.1230	51.083	q *

 $q^{*}$  is the wave vector at the first maximum.

**Table A3.** WAXS data of PXA-*a*-S36.

T (°C)	q (A <sup>-1</sup> )	d (Å)	
30 °C heating	1.5187	4.137	$q_{\rm w}$
70 °C	1.3661	4.599	diffuse
30 °C cooling	1.5174	4.141	$q_{\mathrm{w}}$

**Table A4.** SAXS data of PXA-g-S36.

T (°C)	q (Å-1)	d (Å)	
30 °C heating	0.1648	38.126	q *
	0.3286	19.121	2q *
	0.4903	12.815	3q *
70 °C	0.1676	37.489	Broad Peak
30 °C cooling	0.1649	38.103	q *
	0.3292	19.086	2q *
	0.4896	12.833	3q*

 $<sup>\</sup>mathbf{q}^*$  is the wave vector at the first maximum.

**Table A5.** WAXS data of PDSA-*g*-S10.

T (°C)	q (Å-1)	d (Å)	
30 °C heating	1.4299	4.394	diffuse
S	1.5199	4.134	$\mathbf{q}_{\mathbf{w}}$
70°C	1.3788	4.557	diffuse
30 °C cooling	1.3557	4.635	diffuse
8	1.5015	4.185	$q_{\mathrm{w}}$

**Table A6.** SAXS data of PDSA-*g*-S10.

T (°C)	q (Å-1)	d (Å)	
30 °C heating	0.1100	57.120	q*
70 °C	0.1205	52.143	Broad Peak
30 °C cooling	0.1133	55.456	q *

q\* is the wave vector at the first maximum

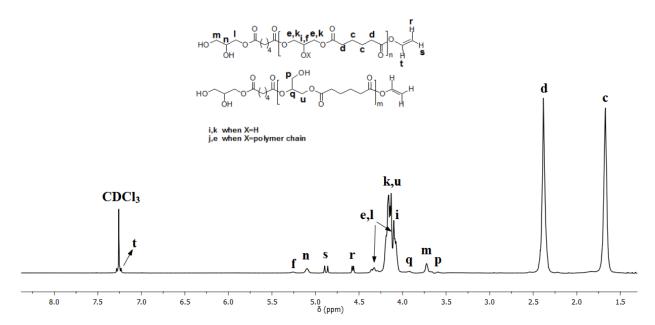
**Table A7**. WAXS data of PDSA-*g*-S68.

T (°C)	q (Å <sup>-1</sup> )	d (Å)	
30 °C heating	1.5150	4.147	$q_{\mathrm{w}}$
70 °C	1.3640	4.606	diffuse
30 °C cooling	1.5123	4.155	$q_{\rm w}$

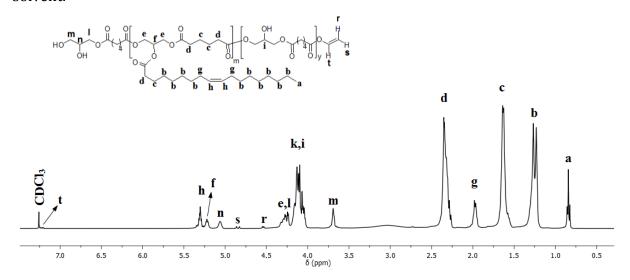
<b>Table A8</b>	. SAXS	data	of PDSA-	g-S68.
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T (°C)	q (Å-1)	d (Å)	
30 °C heating	0.1734	36.235	q *
3	0.3464	18.139	2q *
70 °C	0.1856	33.853	Braod Peak
30 °C cooling	0.1768	35.538	q *
	0.3506	17.921	2q *

 $q^*$  is the wave vector at the first maximum.



**Figure A2.**¹H NMR spectrum of poly(glycerol adipate) recorded at 27°C using CDCl<sub>3</sub> as solvent.



**Figure A3.**¹H NMR spectrum of PGA-g-O22 recorded at 27 °C using CDCl<sub>3</sub> as solvent.

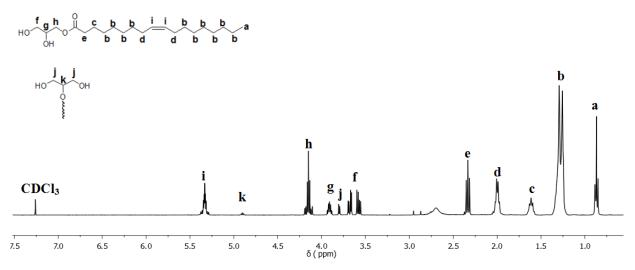
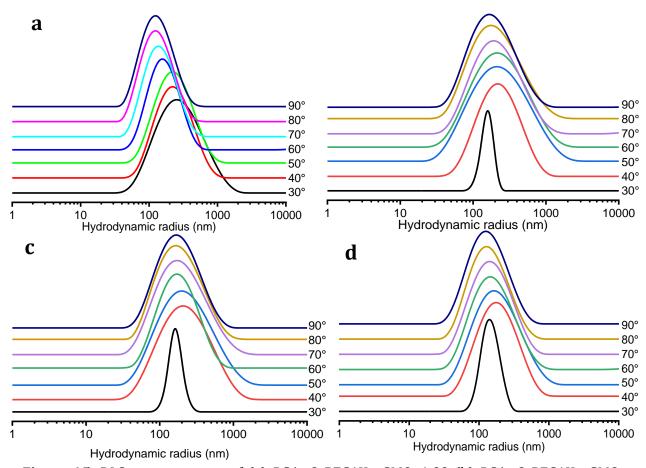
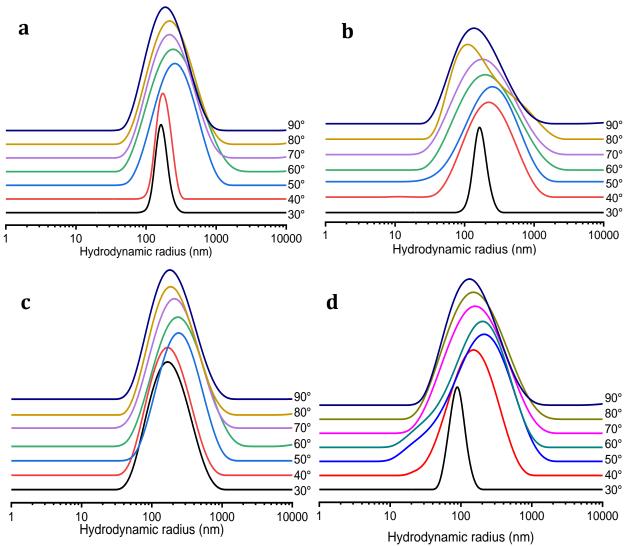


Figure A4. ¹H NMR of spectrum of G1MO and G2MO recorded at 27°C using CDCl3 as solvent.



**Figure A5.** DLS measurements of (a)  $PGA_{26}O_4PEG1K_{17}$ :GMO=1:99 (b)  $PGA_{26}O_4PEG1K_{17}$ :GMO=3:97 (c)  $PGA_{26}O_4PEG1K_{17}$ :GMO=5:95 and (d)  $PGA_{26}O_4PEG1K_{17}$ :GMO=10:90 at 7 different angles.



**Figure A6.** DLS measurements of (a)  $PGA_{26}O_{13}PEG1K_8$ : GMO = 1.99 (b)  $PGA_{26}O_{13}PEG1K_8$ : GMO = 3:97 (c)  $PGA_{26}O_{13}PEG1K_8$ : GMO = 5:95 and (d)  $PGA_{26}O_{13}PEG1K_8$ : GMO = 10:90 at 7 different angles.

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## 9 CURRICULUM VITAE

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#### **10 LIST OF PUBLICATIONS**

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- 2. Jbeily, M.; Naolou, T.; **Bilal, M**.; Amado, E.; Kressler, J. Enzymatically Synthesized Polyesters with Pendent OH Groups as Macroinitiators for the Preparation of Well-Defined Graft Copolymers by Atom Transfer Radical Polymerization. *Polym. Int.* **2014**, *63*, 894–901.
- 3. **Bilal, M. H.**; Prehm, M.; Njau, A.; Samiullah, M.; Meister, A.; Kressler, J. Enzymatic Synthesis and Characterization of Hydrophilic Sugar Based Polyesters and Their Modification with Stearic Acid. *Polymers* **2016**, *8*, 80.
- 4. **Bilal, M. H.**; Hussain, H.; Prehm, M.; Baumeister, U.; Meister, A.; Hause, G.; Busse, K.; Mäder, K.; Kressler, J. Synthesis of Poly(Glycerol Adipate)-*g*-Oleate and Its Ternary Phase Diagram with Glycerol Monooleate and Water. *Eur. Polym. J.* **2017**, *91*, 162–175.

## **Abstracts and posters**

**Bilal, M. H.;** Samiullah, M. H.; Kressler, J. Preparation and characterization of nanoparticles from fatty acid modified polyesters. 248<sup>th</sup> ACS National Meeting, San Francisco, CA. August 2014

**Bilal, M. H.;** Maryam Eivazi; Andrew Njau; Kressler, J. Biodegradable polyesters from renewable resources. 251<sup>st</sup> ACS National Meeting & Exposition, San Diego, CA. March 2016

## 11 SELBSTSTÄNDIGKEITSERKLÄRUNG

Hiermit erkläre ich, dass ich die Ergebnisse der vorliegenden Dissertationsarbeit

Enzymatic synthesis and characterization of grafted polyesters and their use as steric stabilizers for cubosomes

am Institut für Chemie der Martin-Luther Universität Halle-Wittenberg unter Anleitung von Herrn Prof. Dr. Jörg Kreßler selbstständig erarbeitet habe.

Hiermit erkläre in an Eides statt, dass ich die vorliegende Arbeit selbständig und ohne fremde Hilfe verfasst habe. Ich habe keine anderen Quellen und Hilfsmittel als die angegebenen verwendet und anderen Werken wörtlich oder inhaltlich entnommene Stellen als solche gekennzeichnet. Diese Arbeit habe ich an keiner anderen Hochschule vorgelegt und mich zu keinem früheren Zeitpunkt um den Doktorgrad beworben.